

ESE 3400: Medical Devices Lab

Lec 6: October 11, 2023
Data Converters





Lecture Outline

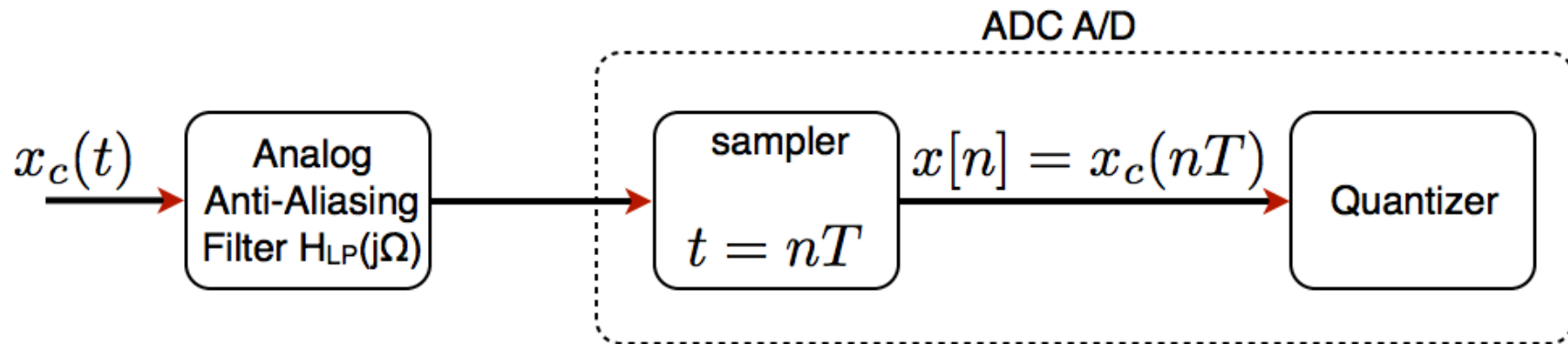
- DTFT vs DFT
- Sampling Examples
- SQNR
- Oversampling
- ADC Architectures
 - Flash ADCs
 - SAR ADCs
 - Delta-Sigma ADCs

ADC

Analog to Digital Converter

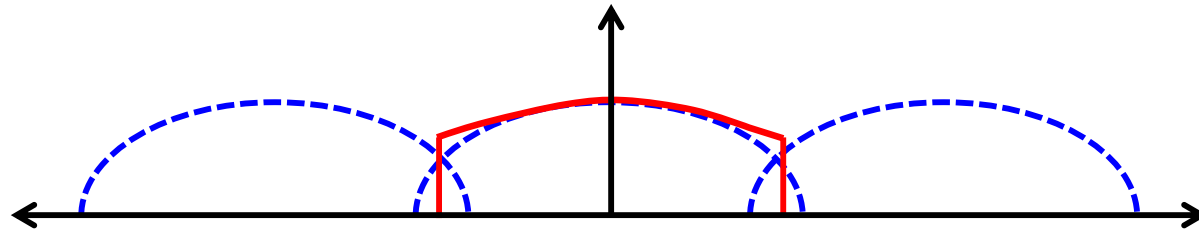


Anti-Aliasing Filter with ADC



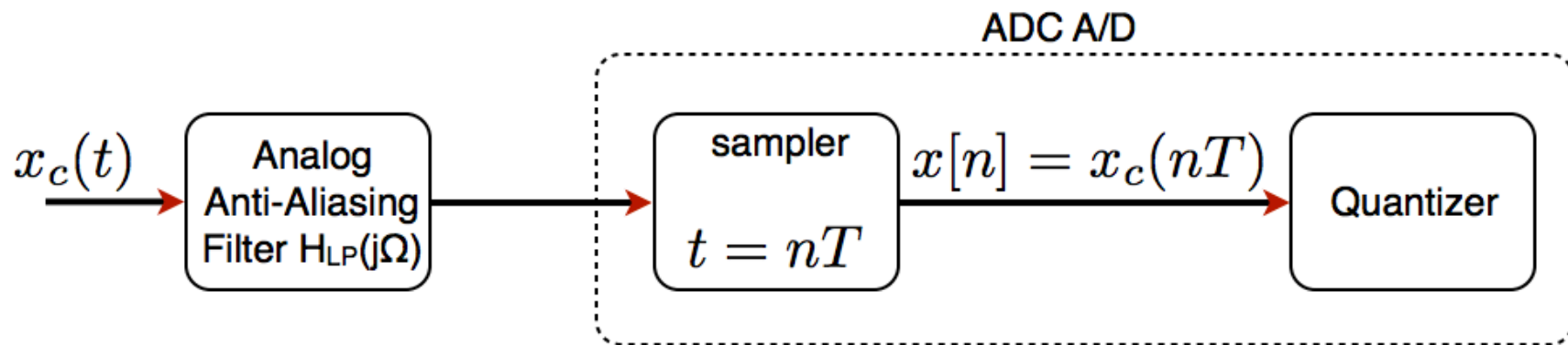
Aliasing

- If $\Omega_N > \Omega_s/2$, $x_r(t)$ an aliased version of $x_c(t)$

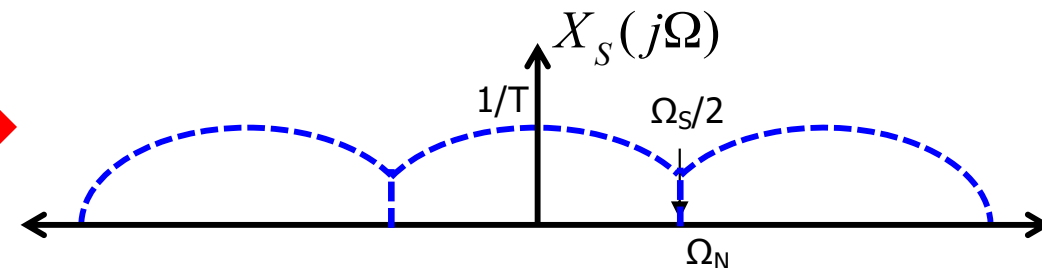
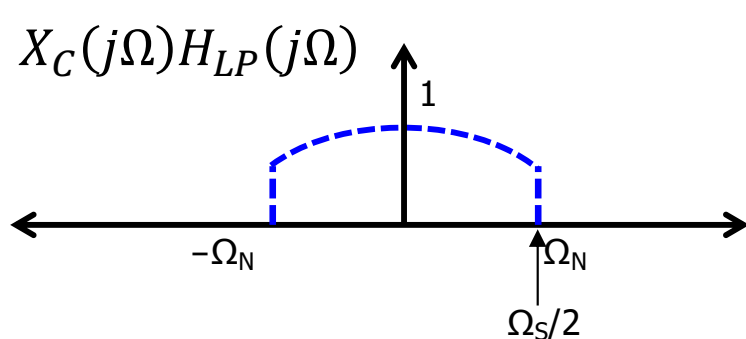
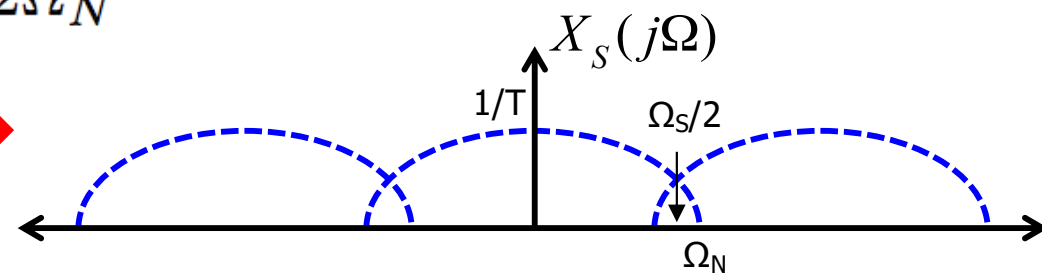
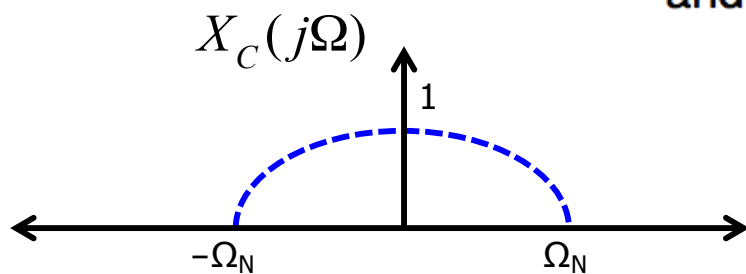


$$X_r(j\Omega) = \begin{cases} TX_s(j\Omega) & \text{if } |\Omega| \leq \Omega_s/2 \\ 0 & \text{otherwise} \end{cases}$$

Anti-Aliasing Filter with ADC



and $\Omega_s < 2\Omega_N$



DTFT Vs. DFT

DTFT:

$$X(e^{j\omega}) = \sum_{k=-\infty}^{\infty} x[k]e^{-j\omega k}$$

$$x[n] = \frac{1}{2\pi} \int_{-\pi}^{\pi} X(e^{j\omega})e^{j\omega n} d\omega$$

DFT:

$$x[n] = \frac{1}{N} \sum_{k=0}^{N-1} X[k]W_N^{-kn}$$

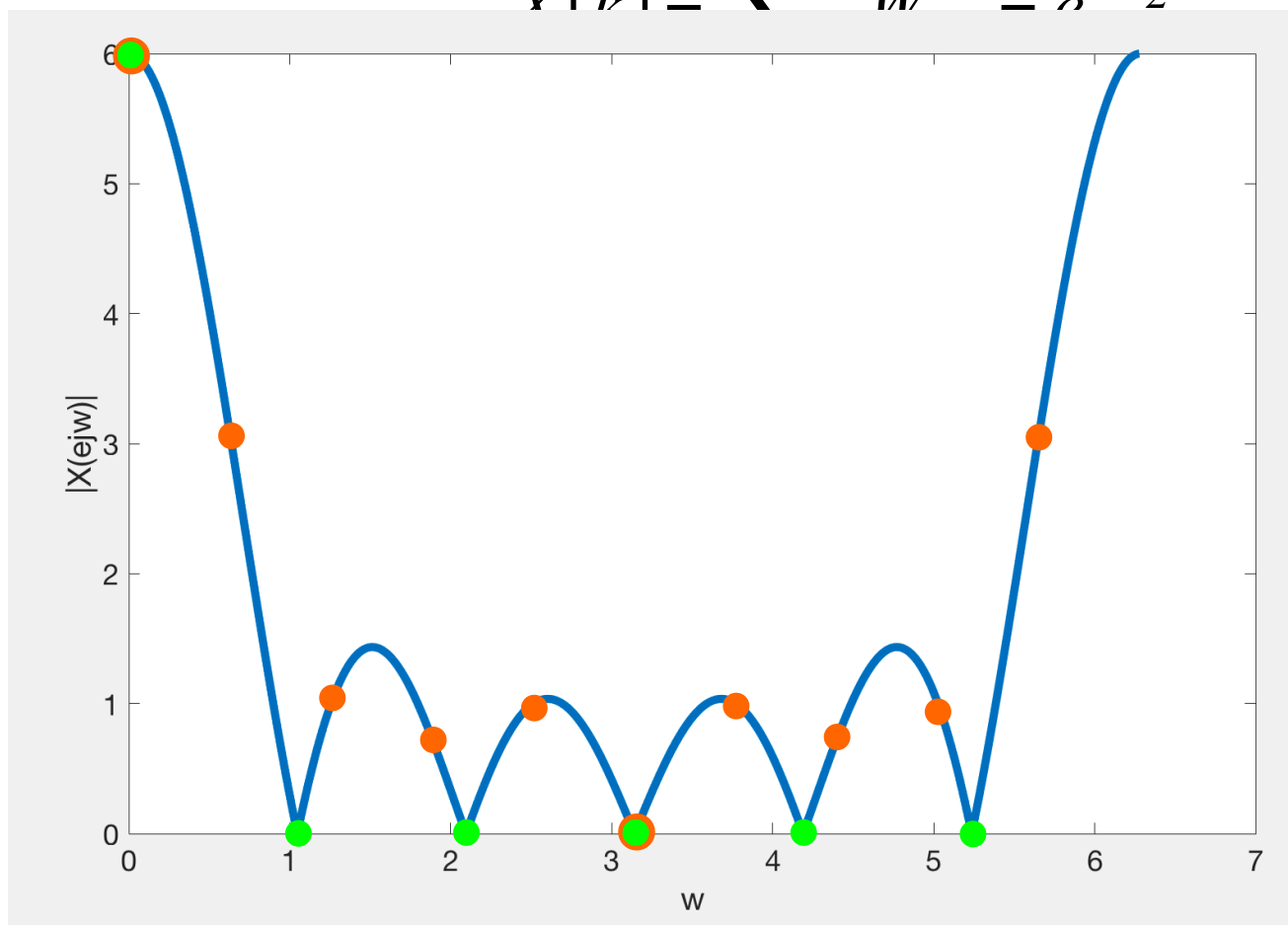
$$X[k] = \sum_{n=0}^{N-1} x[n]W_N^{kn}$$



DFT vs DTFT

□ Back to example

$$X[k] = \sum_{n=0}^5 W^{nk} = \sum_{n=0}^5 e^{-j\frac{\pi}{2}nk} = \frac{\sin\left(\frac{3\pi}{5}k\right)}{\sin\left(\frac{\pi}{10}k\right)}$$



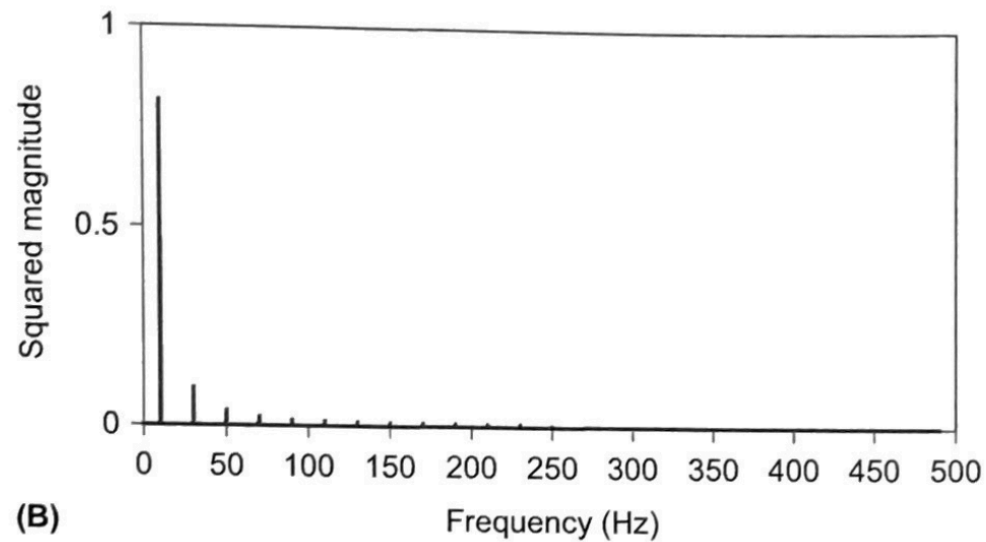
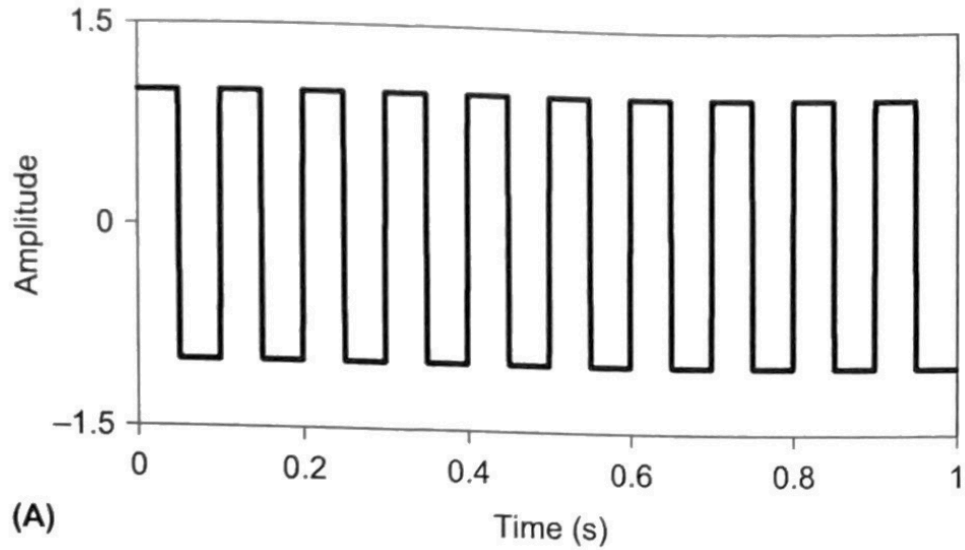
“6-point” DFT

“10-point” DFT

Use `fftshift`
to center
around dc

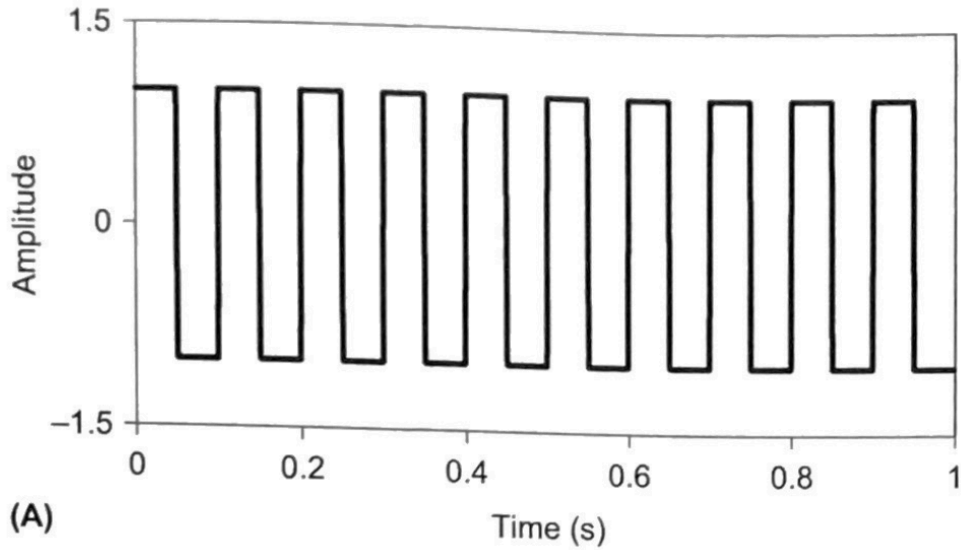


Sampling/Reconstruction Example

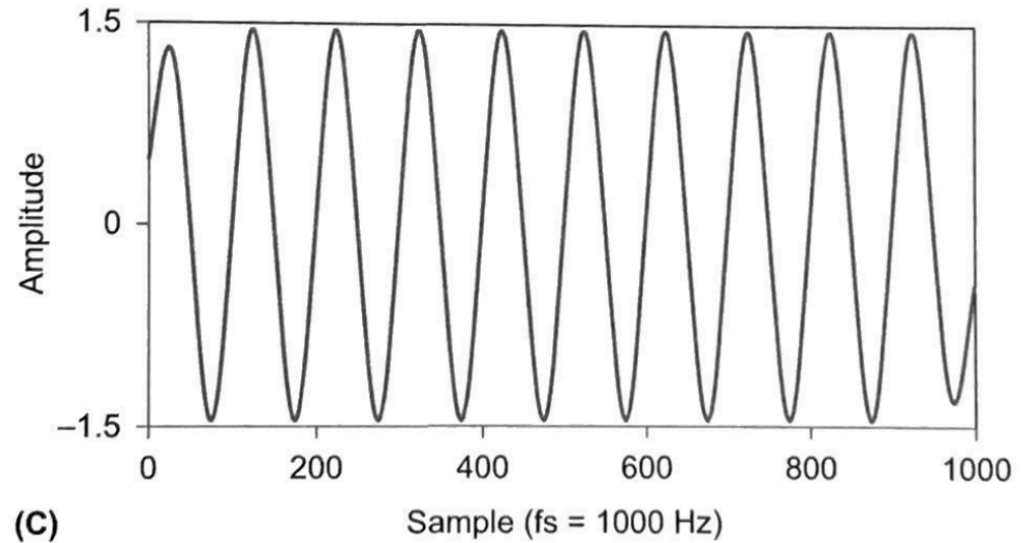




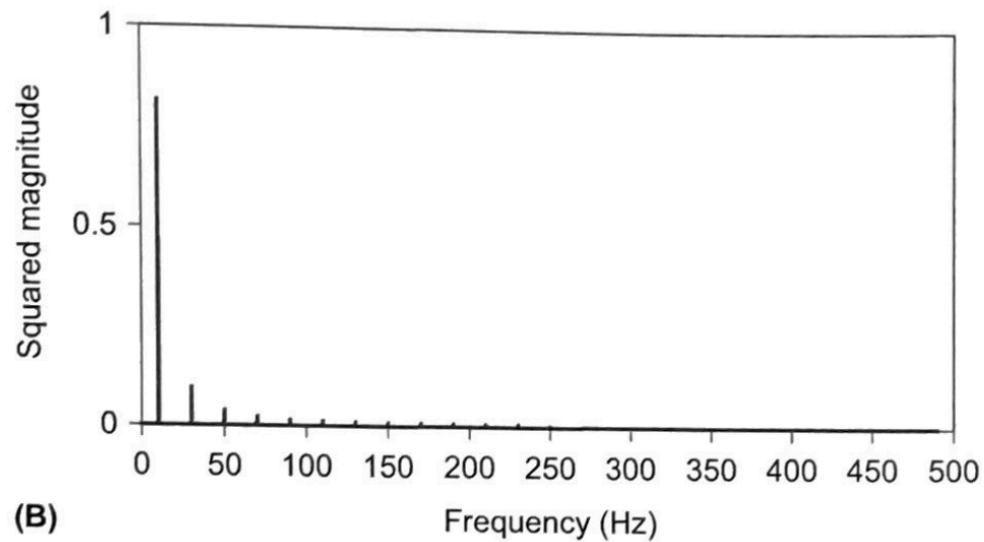
Sampling/Reconstruction Example



(A)

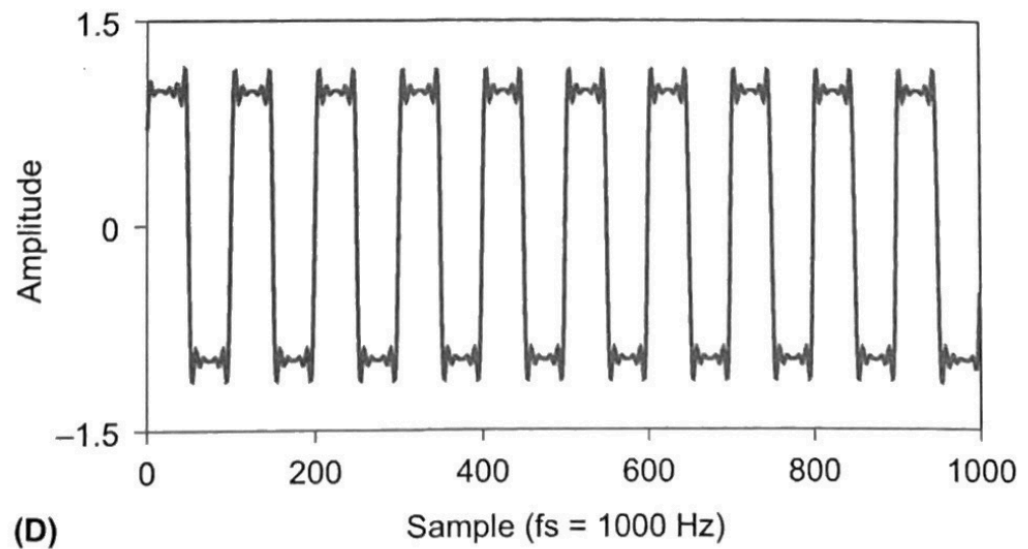
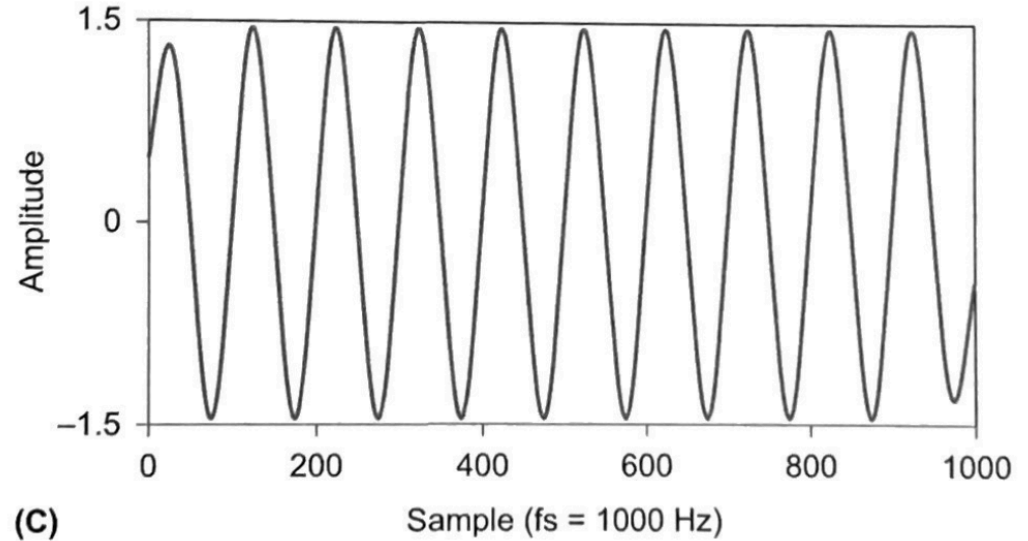
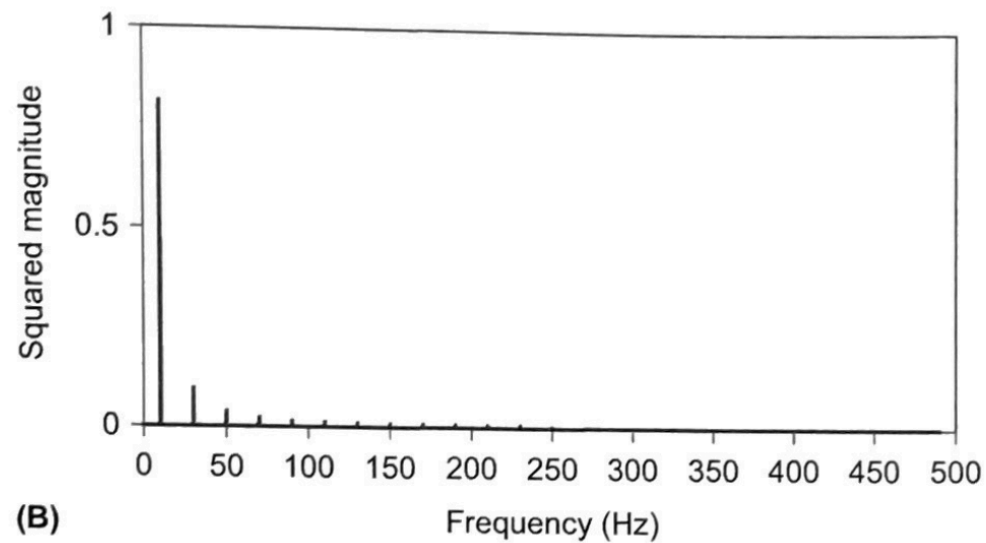
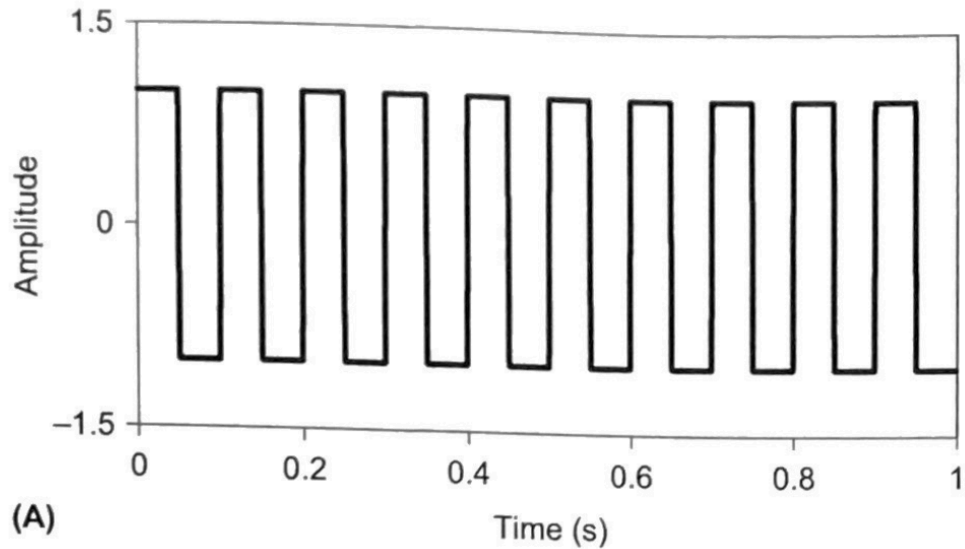


(C)



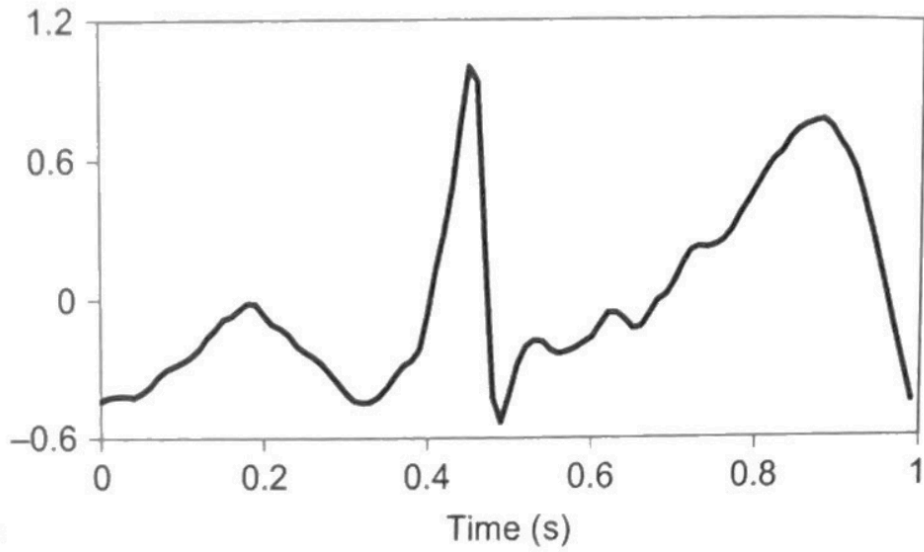
(B)

Sampling/Reconstruction Example

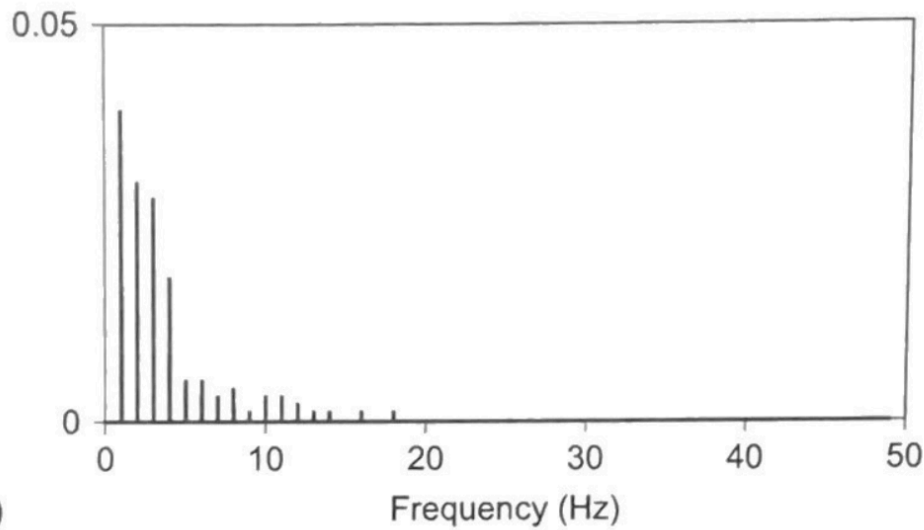




ECG Example



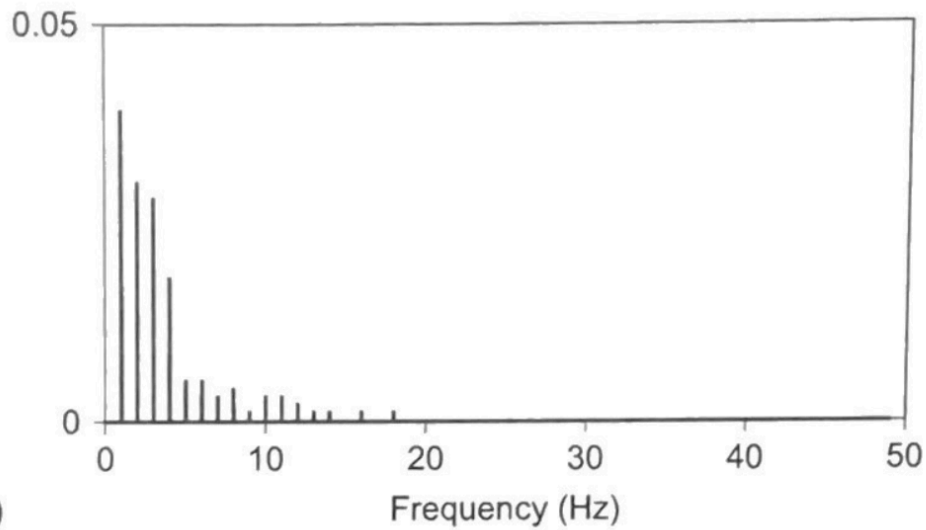
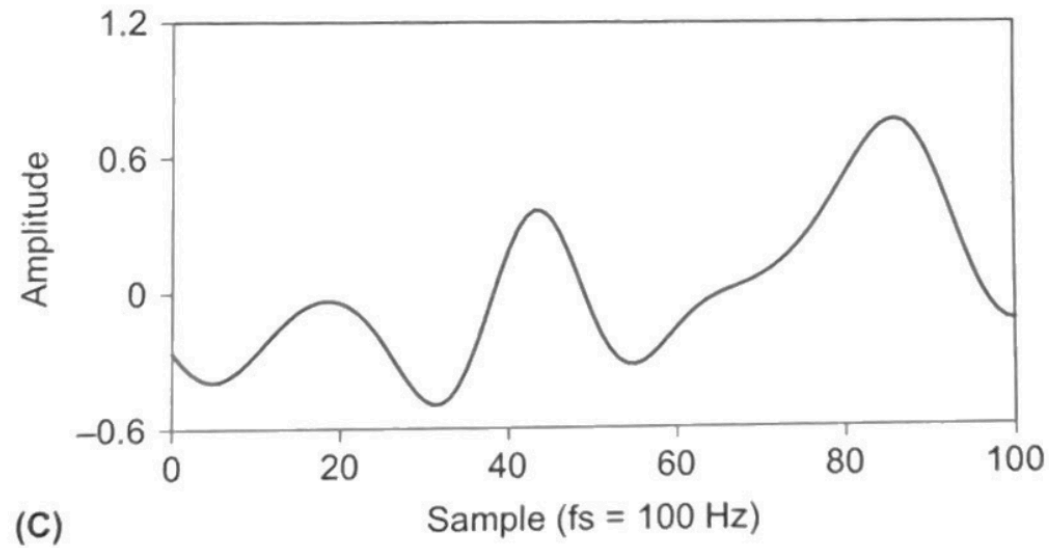
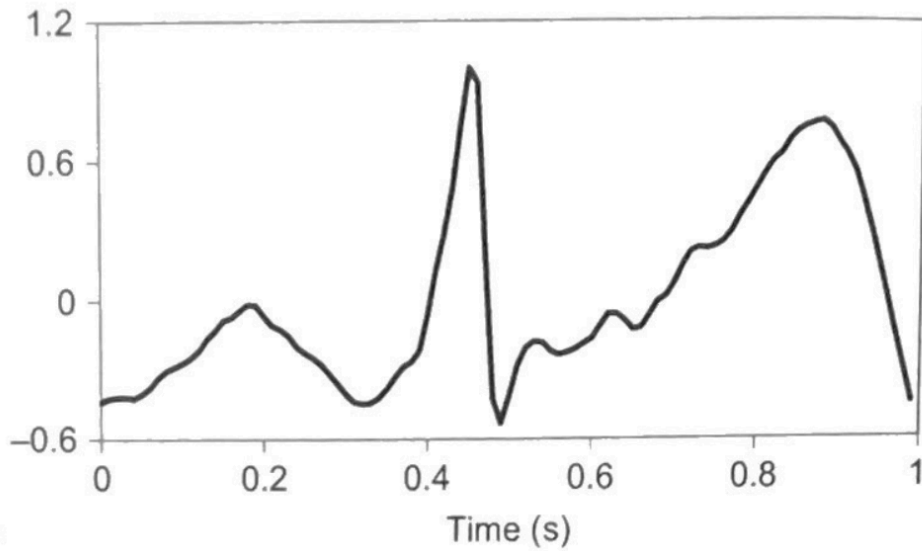
(A)



(B)

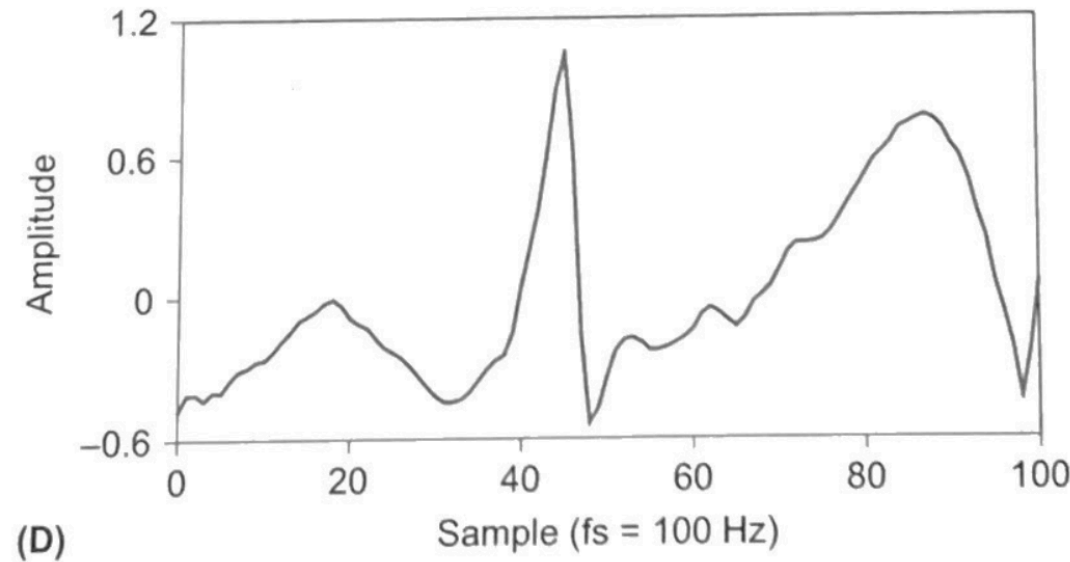
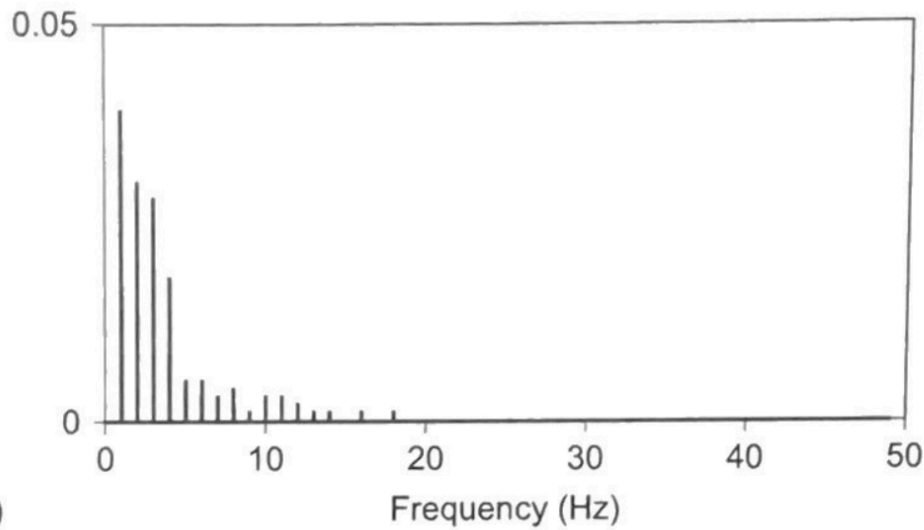
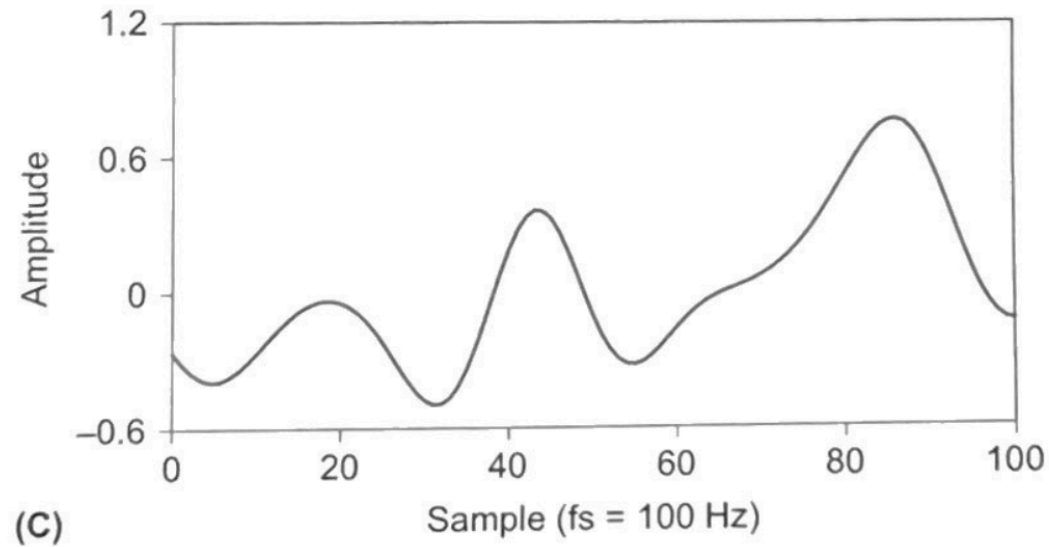
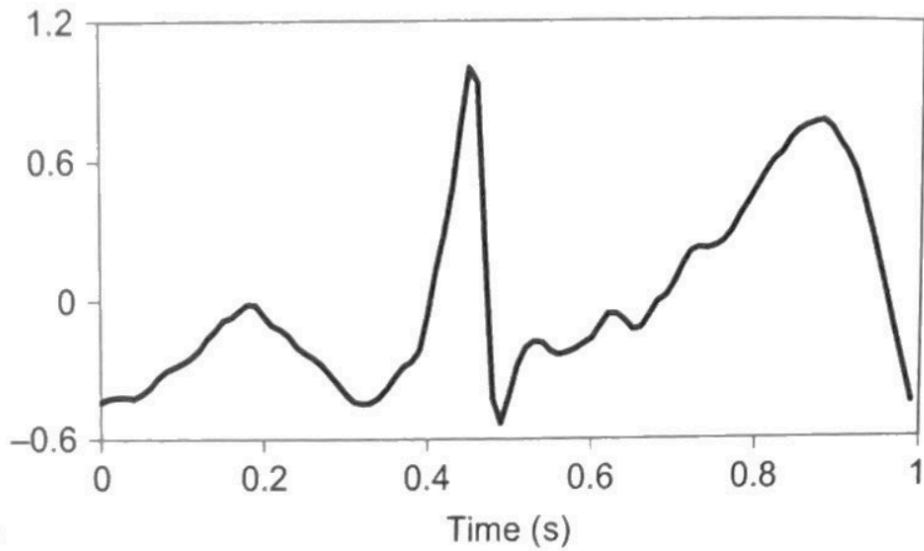


ECG Example

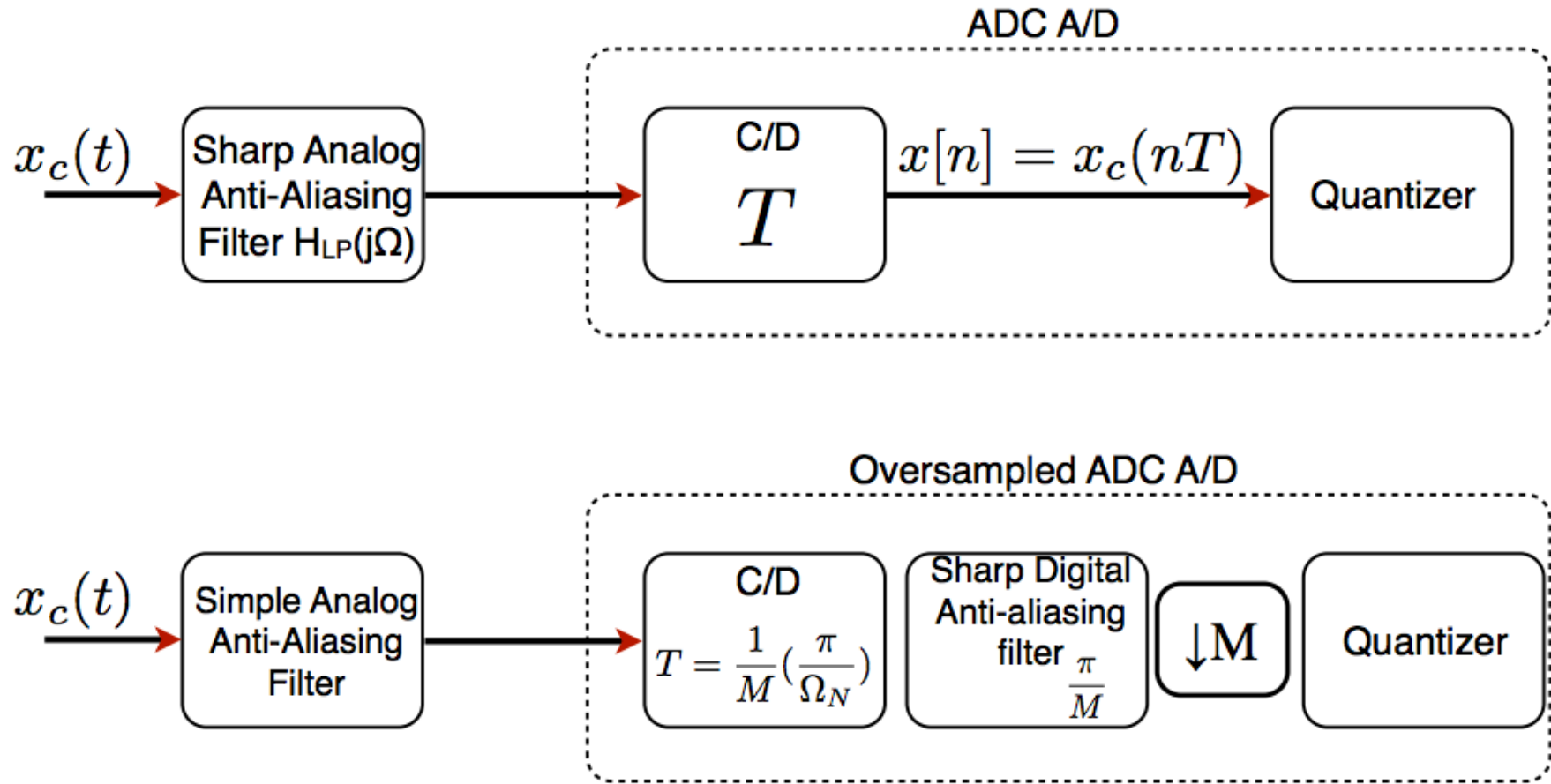




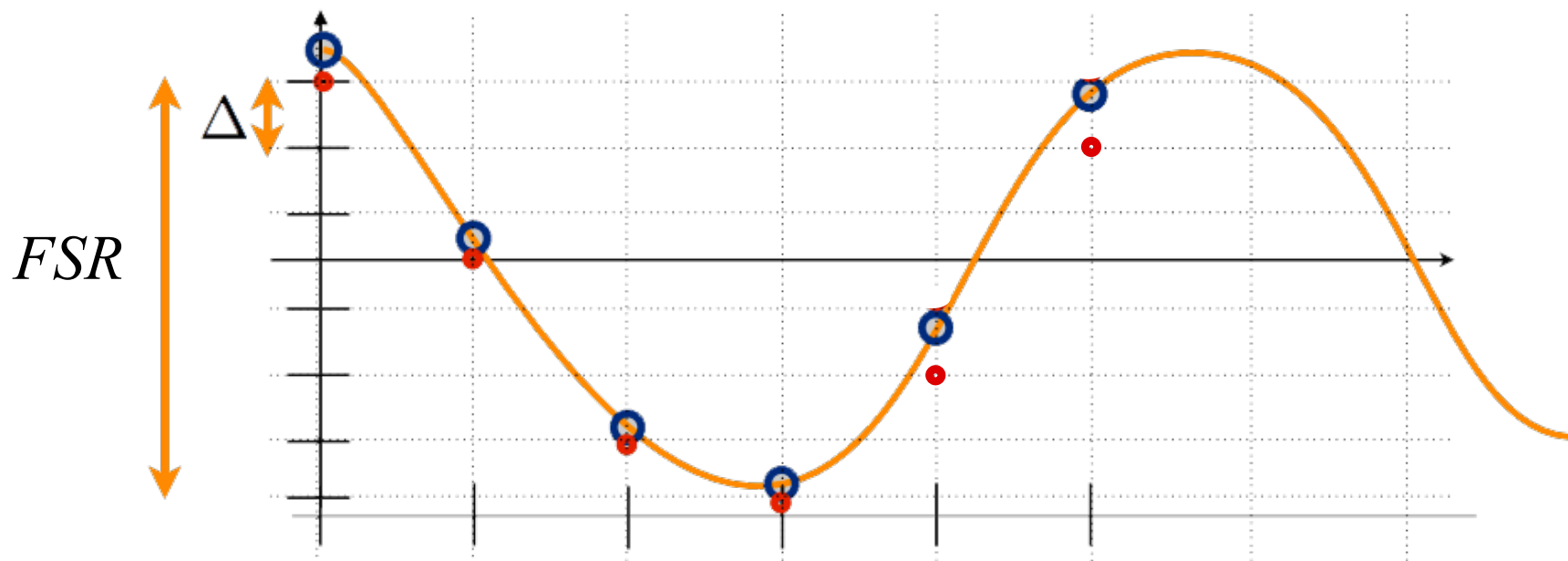
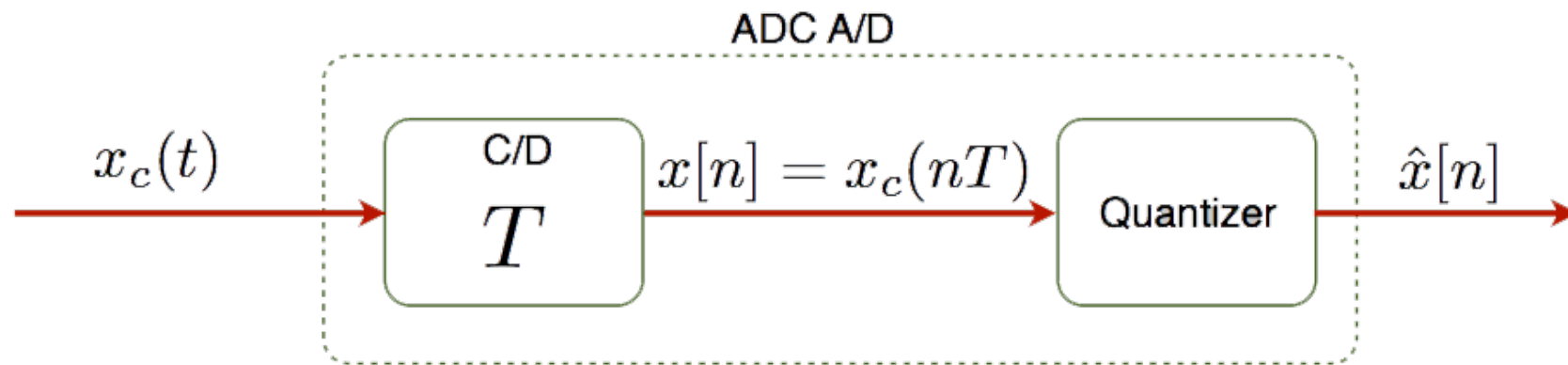
ECG Example



Oversampled ADC



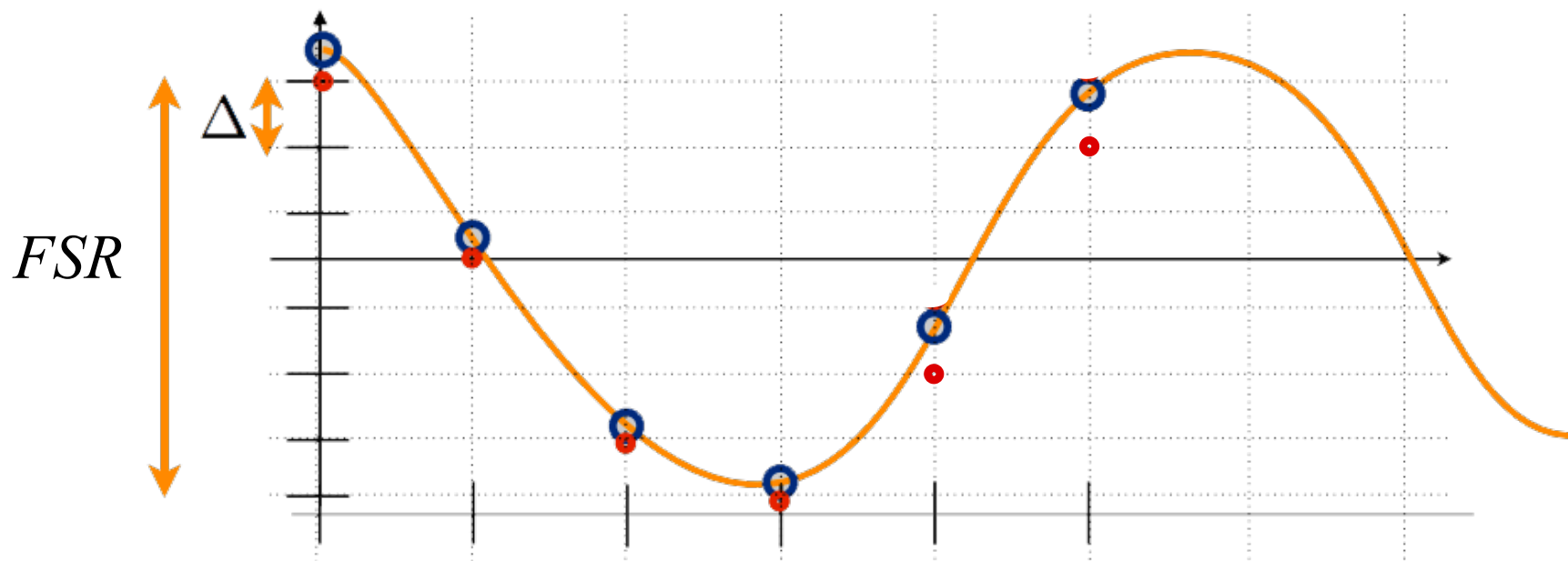
Sampling and Quantization



Sampling and Quantization

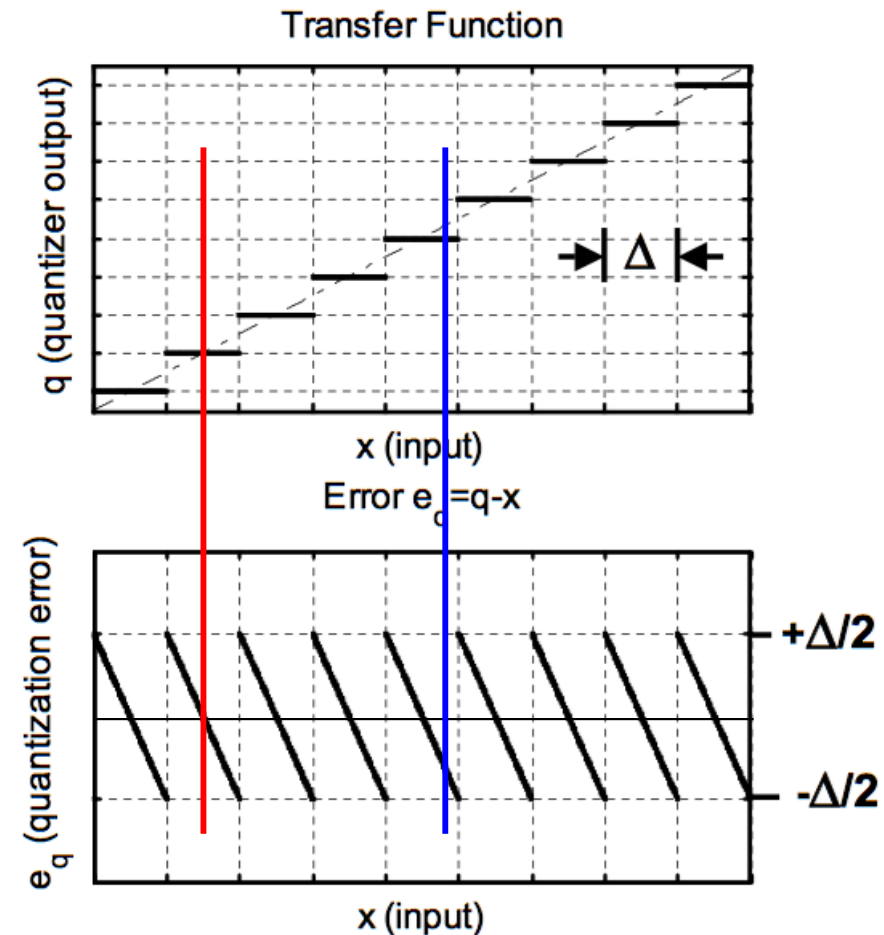
- For an input signal with $V_{pp} = FSR$ with B bits

$$\Delta = \frac{FSR}{2^B}$$



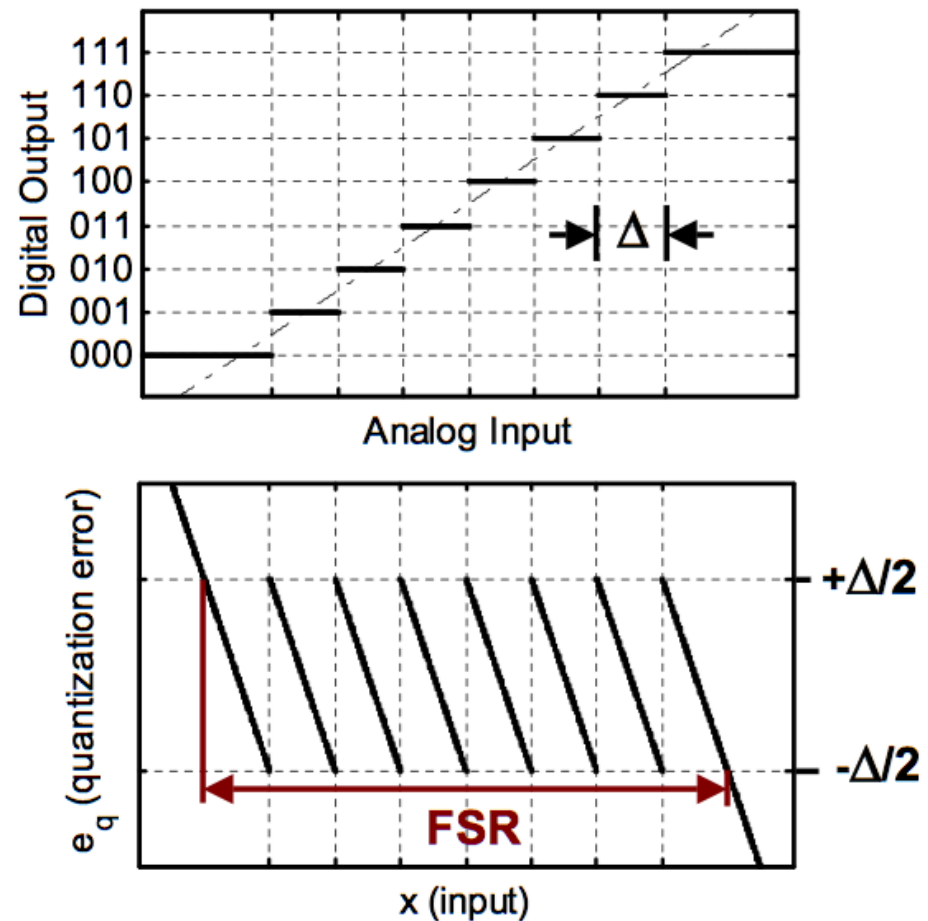
Ideal Quantizer

- Quantization step Δ
- Quantization error has sawtooth shape
 - Bounded by $-\Delta/2$, $+\Delta/2$
- Ideally infinite input range and infinite number of quantization levels



Ideal B-bit Quantizer

- ❑ Practical quantizers have a limited input range and a finite set of output codes
- ❑ E.g. a 3-bit quantizer can map onto $2^3=8$ distinct output codes
- ❑ Quantization error grows out of bounds beyond code boundaries
- ❑ We define the full scale range (FSR) as the maximum input range that satisfies $|e_q| \leq \Delta/2$
 - Implies that $FSR = 2^B \cdot \Delta$



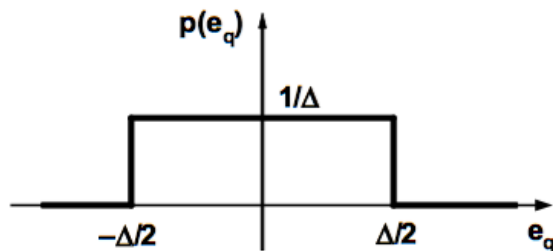


Effect of Quantization Error on Signal

- ❑ Quantization error is a deterministic function of the signal
 - Consequently, the effect of quantization strongly depends on the signal itself
- ❑ Unless, we consider fairly trivial signals, a deterministic analysis is usually impractical
 - More common to look at errors from a statistical perspective
 - "Quantization noise"

Quantization Error Statistics

- ❑ Crude assumption: $e_q(x)$ has uniform probability density
- ❑ This approximation holds reasonably well in practice when
 - Signal spans large number of quantization steps
 - Signal is "sufficiently active"
 - Quantizer does not overload



Mean

$$\bar{e} = \int_{-\Delta/2}^{+\Delta/2} \frac{e}{\Delta} de = 0$$

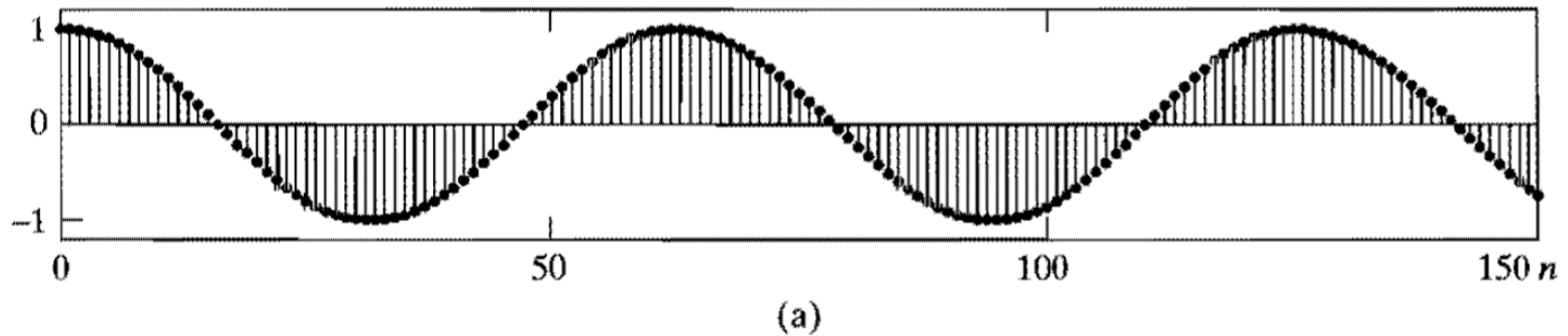
Variance

$$\overline{e^2} = \int_{-\Delta/2}^{+\Delta/2} \frac{e^2}{\Delta} de = \frac{\Delta^2}{12}$$



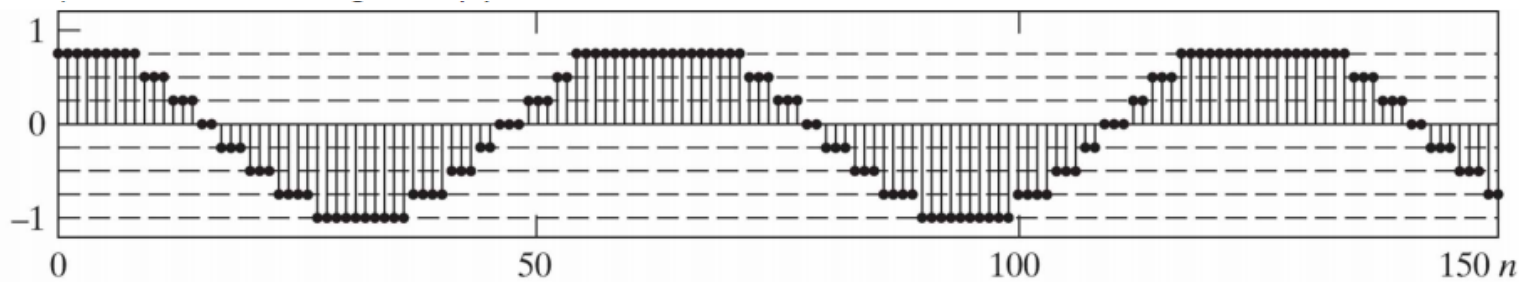
Quantization Noise

- **Figure 4.57** Example of quantization noise. (a) Unquantized samples of the signal $x[n] = 0.99\cos(n/10)$.

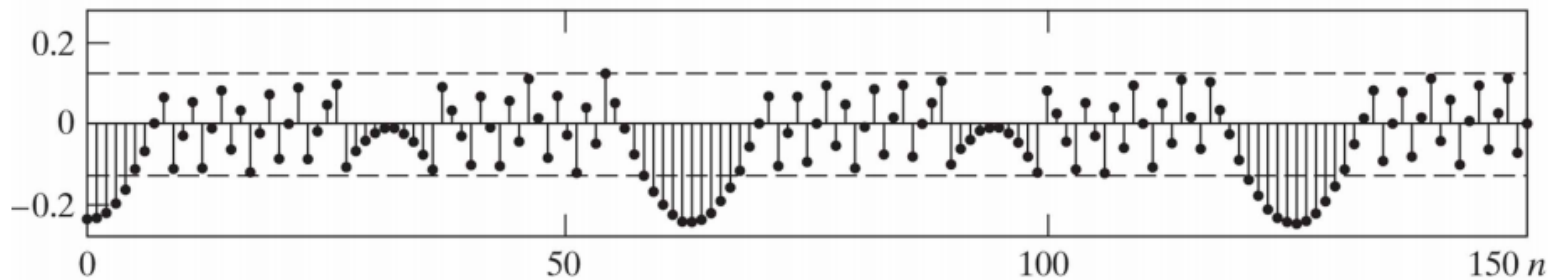


Quantization Noise

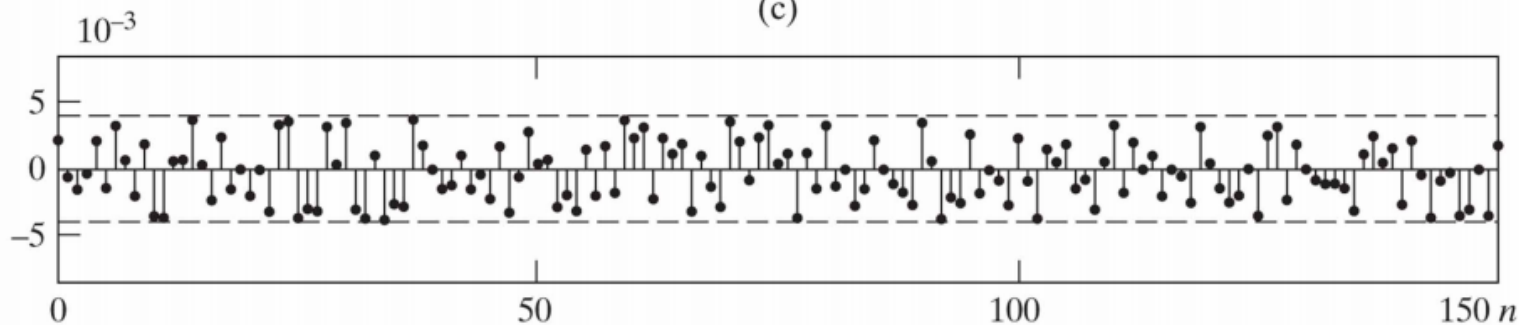
- Figure 4.57(continued) (b) Quantized samples of the cosine waveform in part (a) with a 3-bit quantizer. (c) Quantization error sequence for 3-bit quantization of the signal in (a). (d) Quantization error sequence for 8-bit quantization of the signal in (a).



(b)



(c)



(d)



Signal-to-Quantization-Noise Ratio

- Assuming full-scale sinusoidal input, we have

$$\text{SNR}_Q = 6.02B + 1.76 \text{ dB}$$

B (Number of Bits)	SQNR
8	50dB
12	74dB
16	98dB
20	122dB



Signal-to-Quantization-Noise Ratio

- For uniform B bits quantizer

$$SNR_Q = 10 \log_{10} \left(\frac{\sigma_x^2}{\sigma_e^2} \right)$$

Signal-to-Quantization-Noise Ratio

- For uniform B bits quantizer

$$\begin{aligned} SNR_Q &= 10 \log_{10} \left(\frac{\sigma_x^2}{\sigma_e^2} \right) \\ &= 10 \log_{10} \left(\frac{12 \cdot 2^{2B} \sigma_x^2}{FSR^2} \right) \end{aligned}$$

$$SNR_Q = 6.02B + 10.8 - 20 \log_{10} \left(\frac{FSR}{\sigma_x} \right) \begin{matrix} \text{Quantizer range} \\ \text{rms of amp} \end{matrix}$$



Signal-to-Quantization-Noise Ratio

- Assuming full-scale sinusoidal input, we have

$$\text{SNR}_Q = 6.02B + 10.8 - 20 \log_{10} \left(\frac{\text{Quantizer range}}{\sigma_x \text{ rms of amp}} \right)$$



Signal-to-Quantization-Noise Ratio

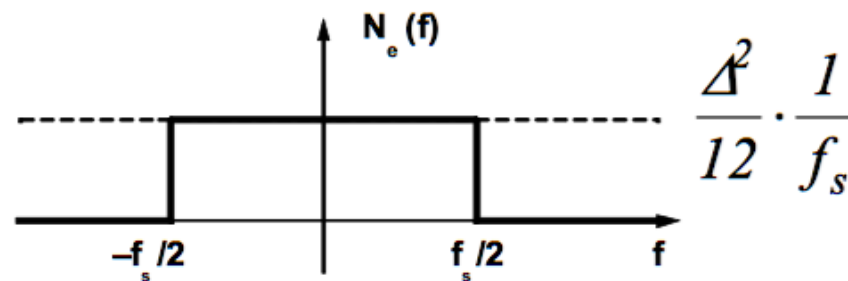
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Quantization Noise Spectrum

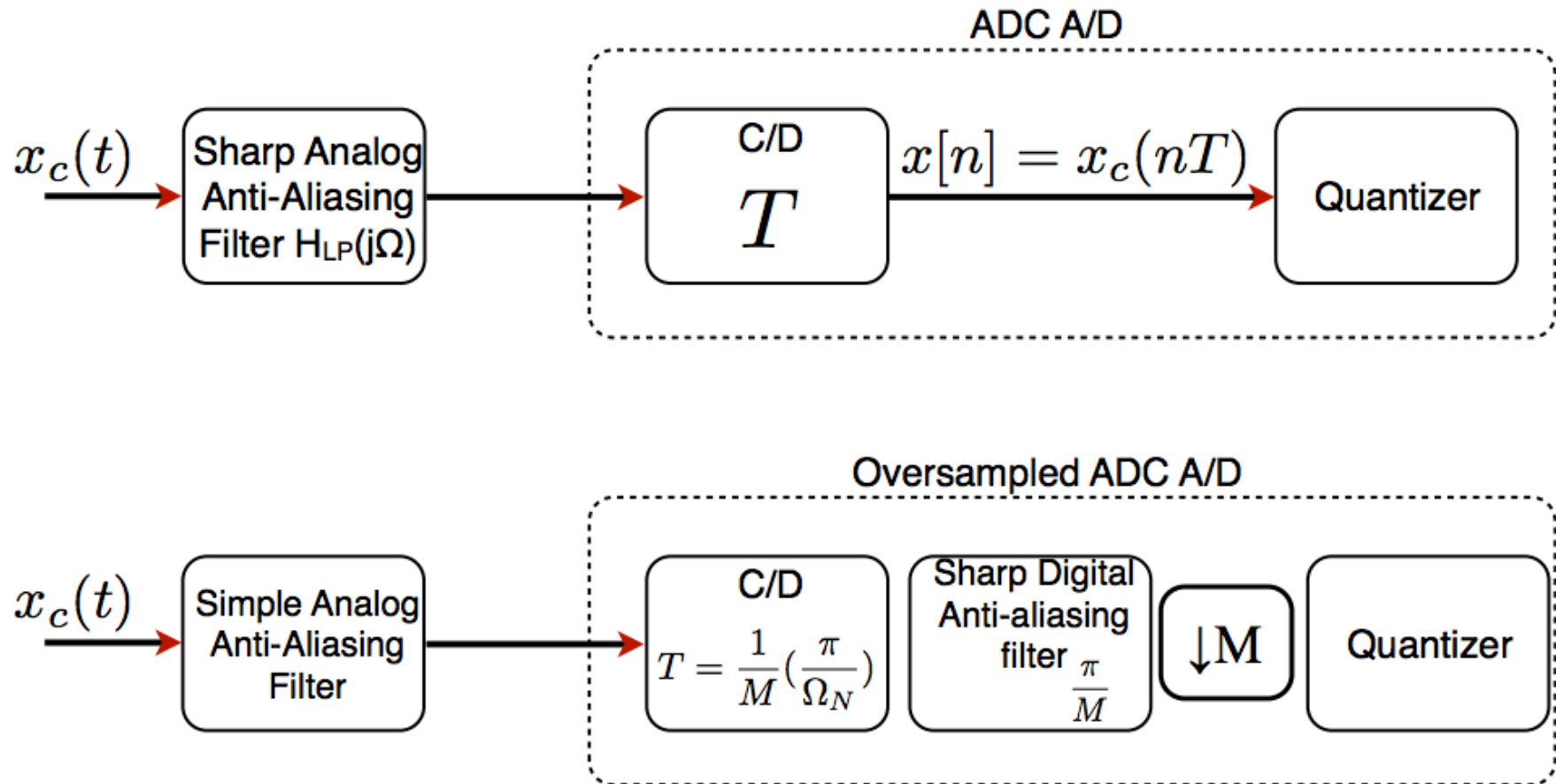
- If the quantization error is "sufficiently random", it also follows that the noise power is uniformly distributed in frequency



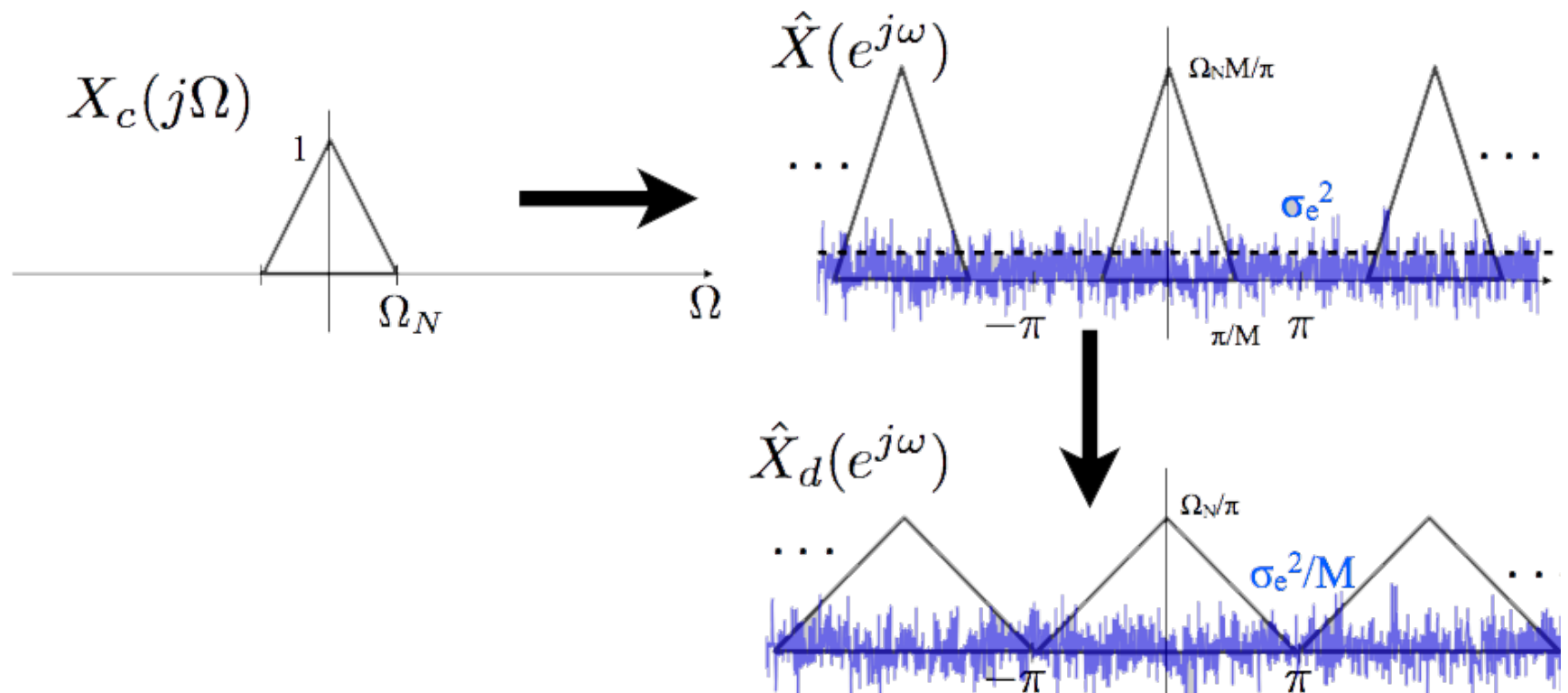
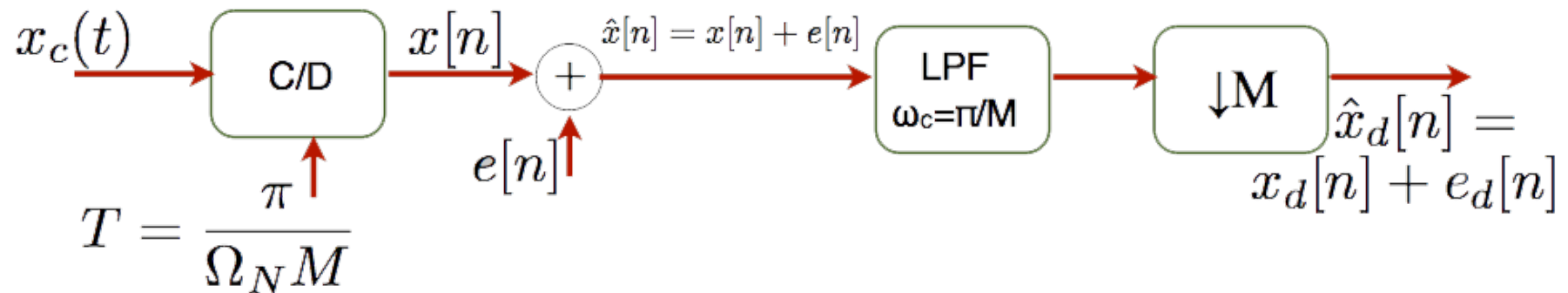
- References

- W. R. Bennett, "Spectra of quantized signals," Bell Syst. Tech. J., pp. 446-72, July 1988.
- B. Widrow, "A study of rough amplitude quantization by means of Nyquist sampling theory," IRE Trans. Circuit Theory, vol. CT-3, pp. 266-76, 1956.

Oversampled ADC



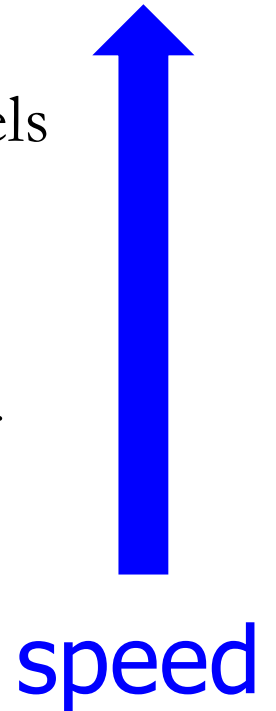
Quantization Noise with Oversampling



ADC Architectures

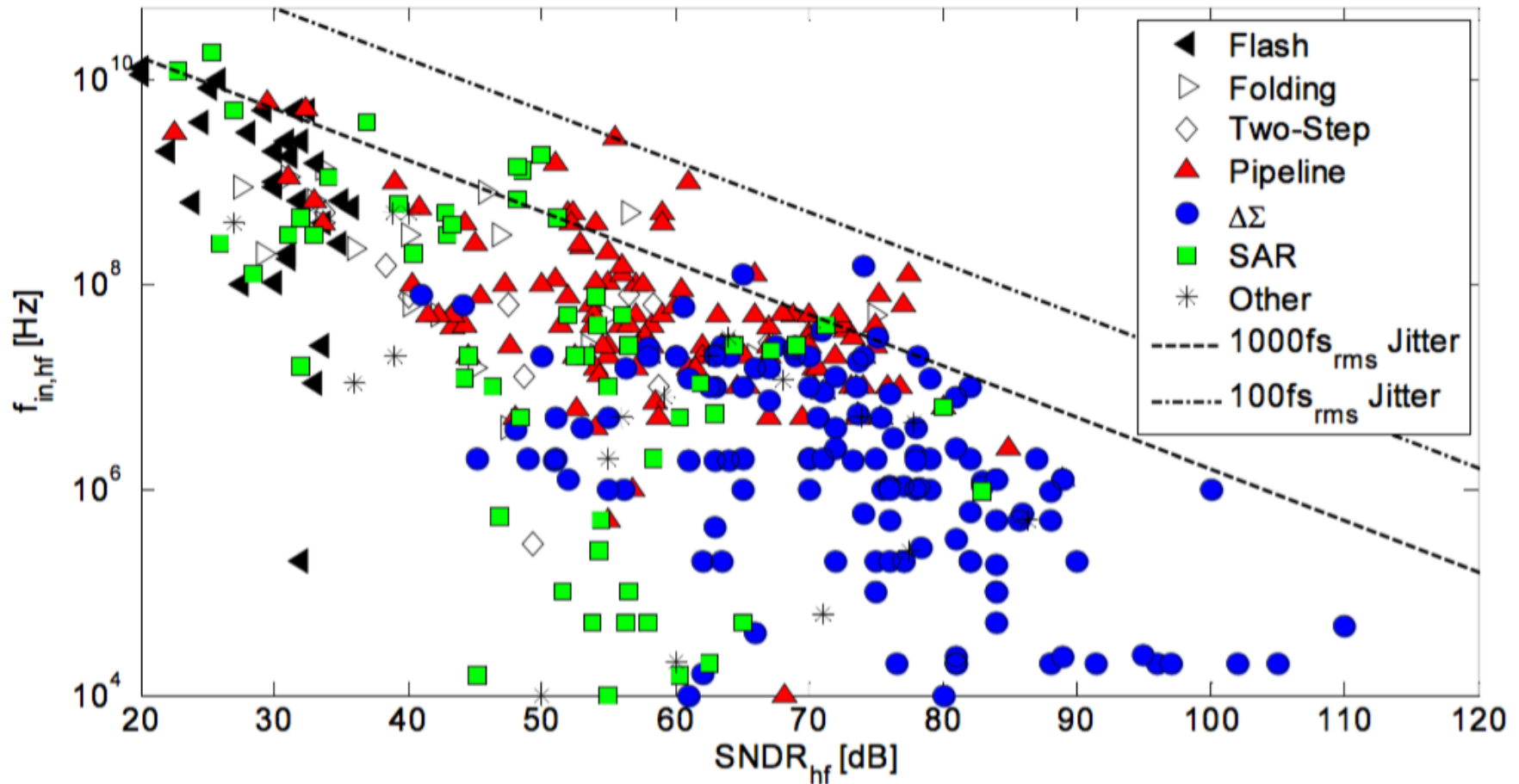
Nyquist ADC Architectures

- Word-at-a-time
 - E.g. flash ADC
 - Instantaneous comparison with 2^B-1 reference levels
- Multi-step
 - E.g. pipeline ADCs
 - Coarse conversion, followed by fine conversion of residuals
- Bit-at-a-time
 - E.g. successive approximation ADCs
 - Conversion via a binary search algorithm



ADC Survey (ISSCC & VLSI 1997-2013)

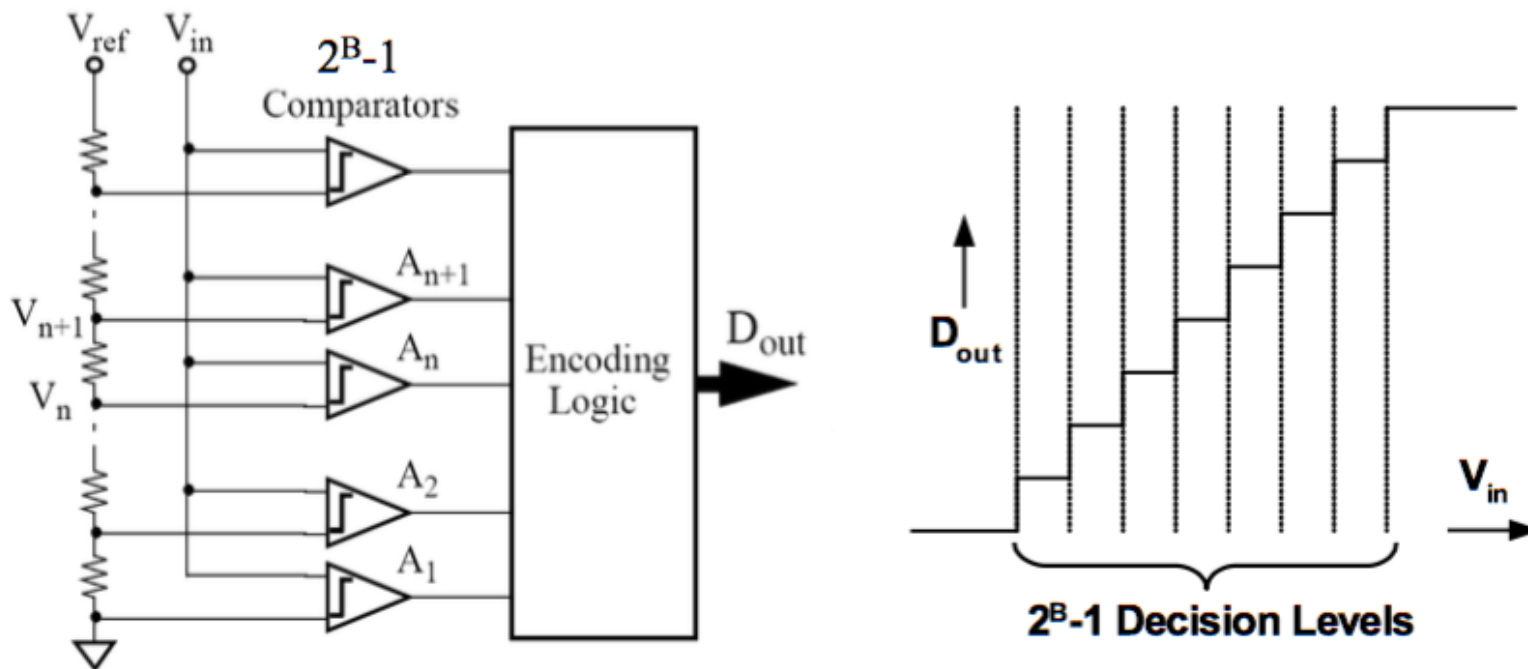
Data: <http://www.stanford.edu/~murmman/adcsurvey.html>



Flash ADCs

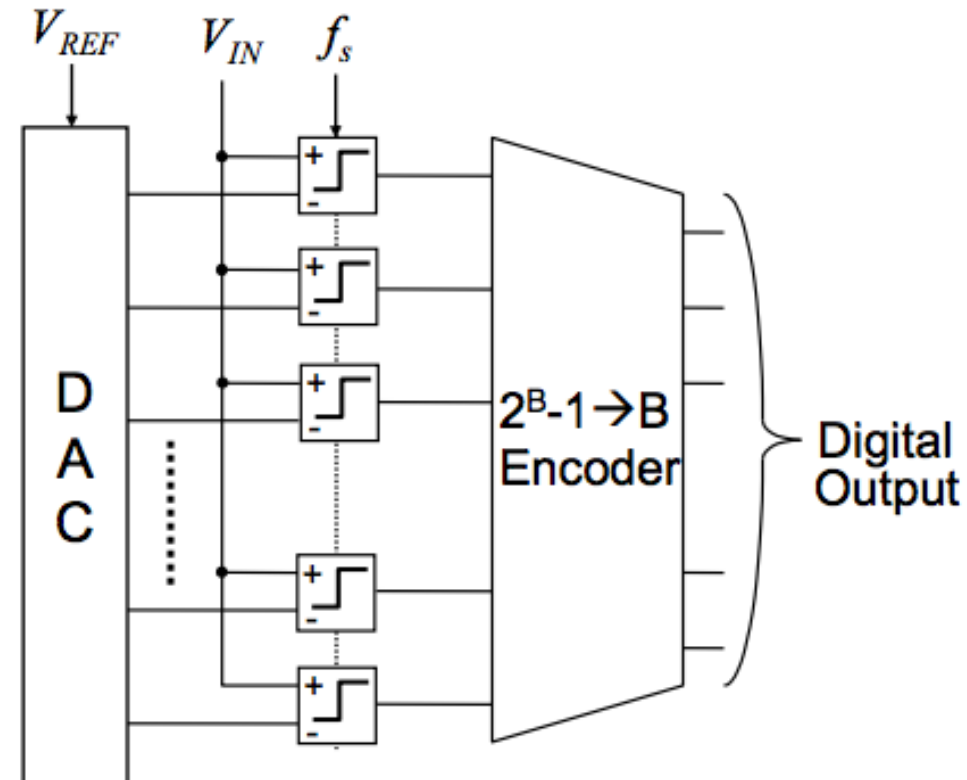
Flash ADC

- ❑ Fast
 - Speed limited by single comparator plus encoding logic
- ❑ High circuit complexity ($2^B - 1$ comparators), high input capacitance
 - Typically only use for resolution up to 6...8 bits

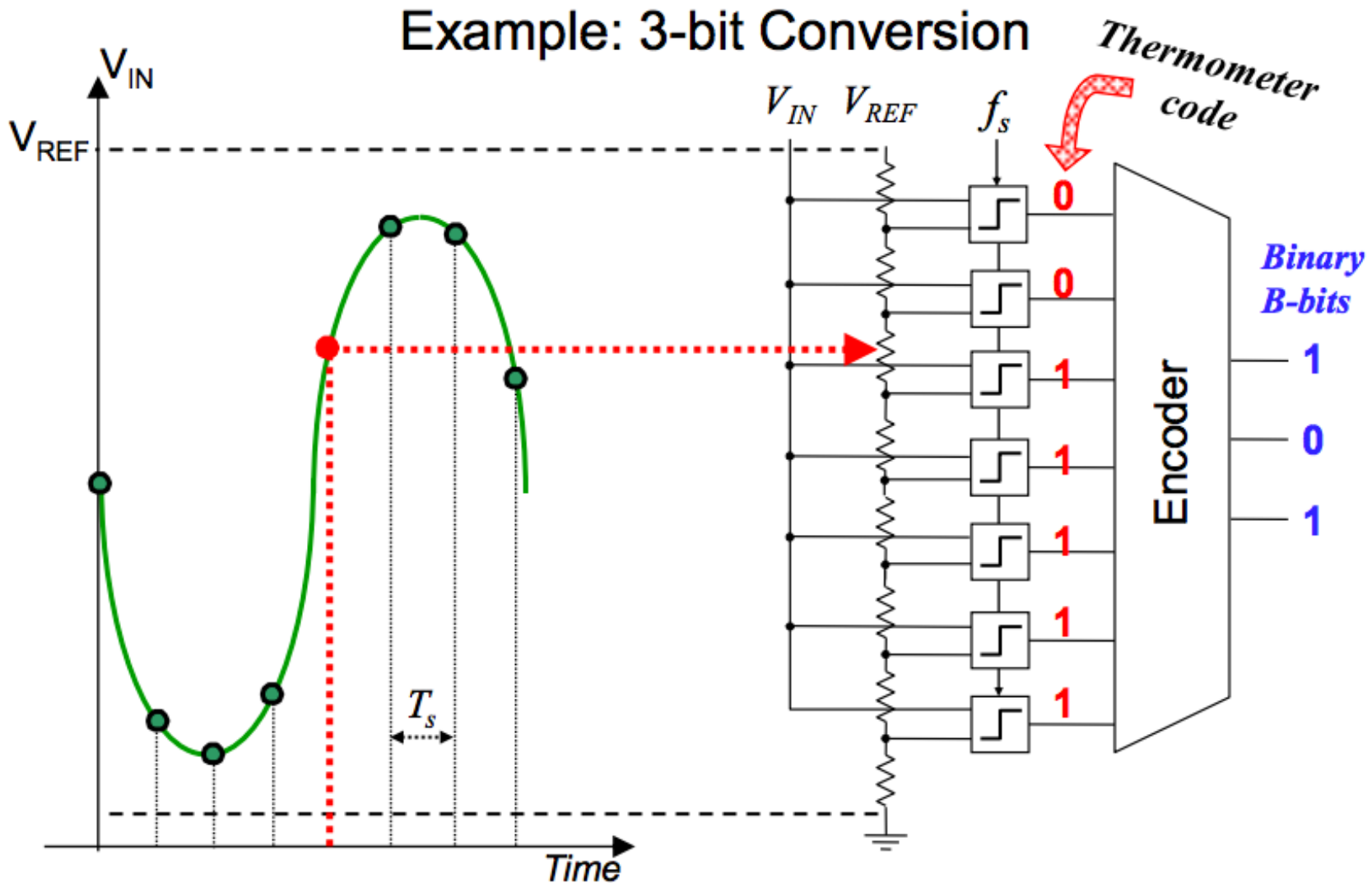


Flash ADC

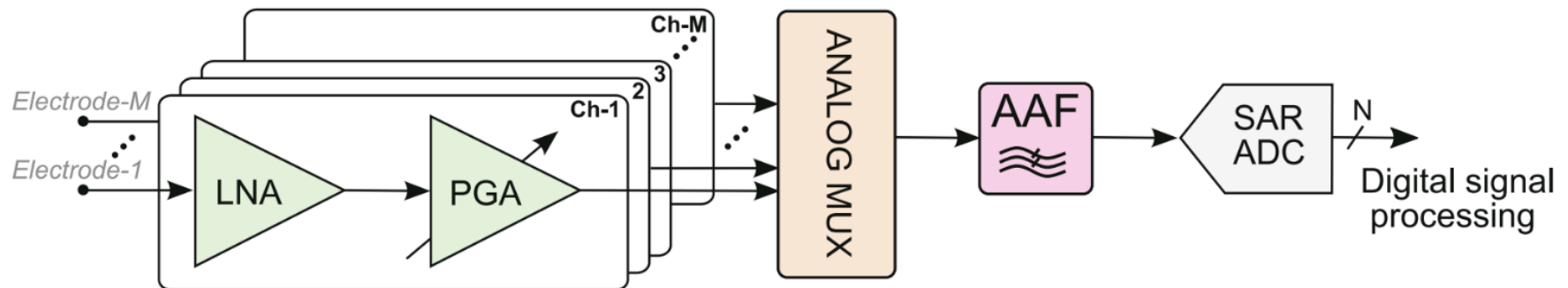
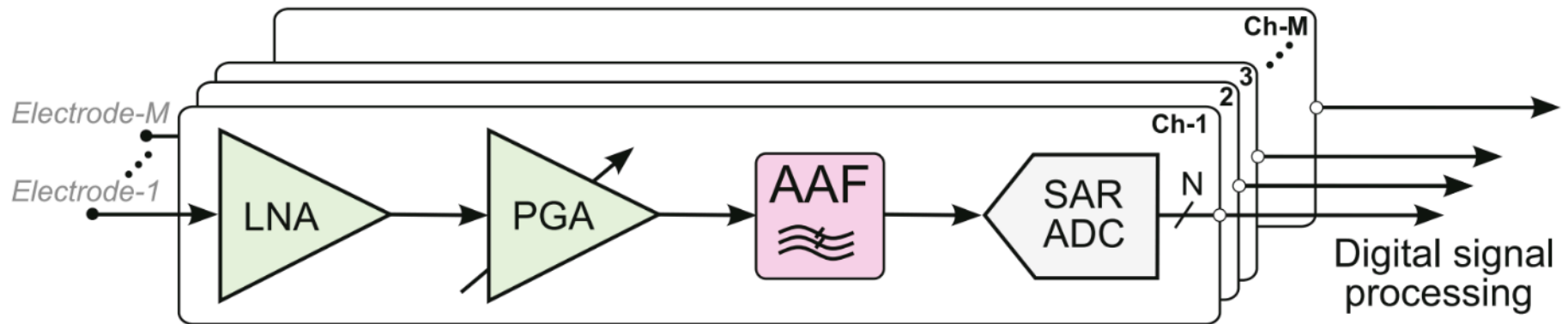
- B-bit flash ADC:
 - DAC generates all possible 2^B-1 levels
 - 2^B-1 comparators compare V_{IN} to DAC outputs
 - Comparator output:
 - If $V_{DAC} < V_{IN} \rightarrow 1$
 - If $V_{DAC} > V_{IN} \rightarrow 0$
 - Comparator outputs form thermometer code
 - Encoder converts thermometer to binary code



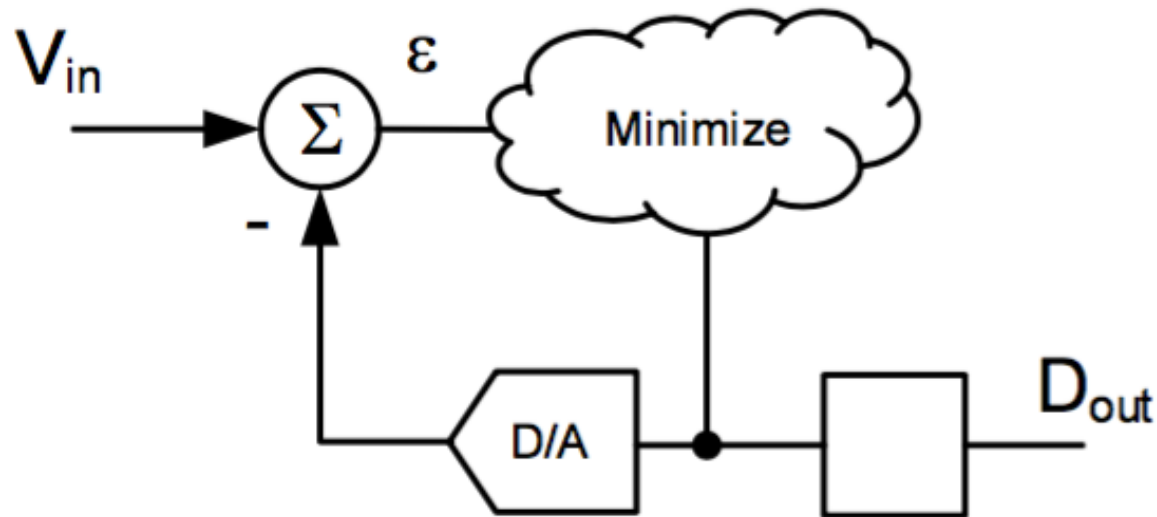
Flash ADC



Multi-channel Bio-potential Recording

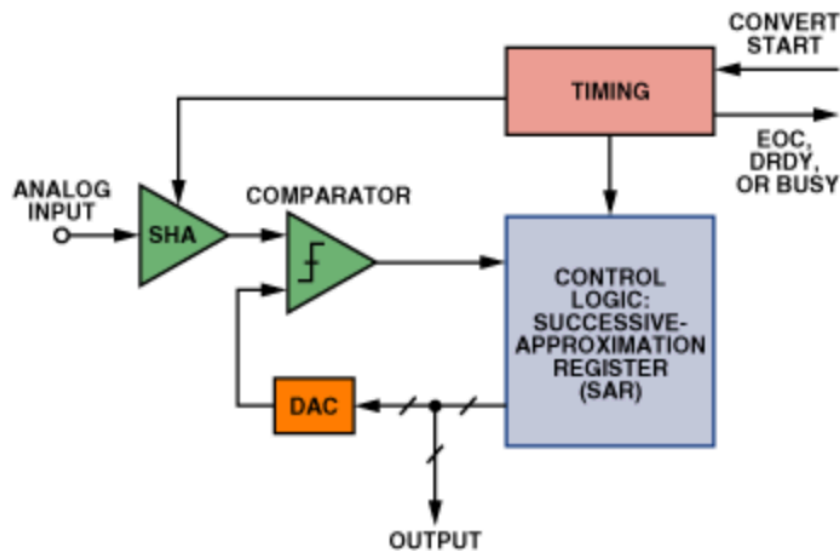


SAR ADC Architectures



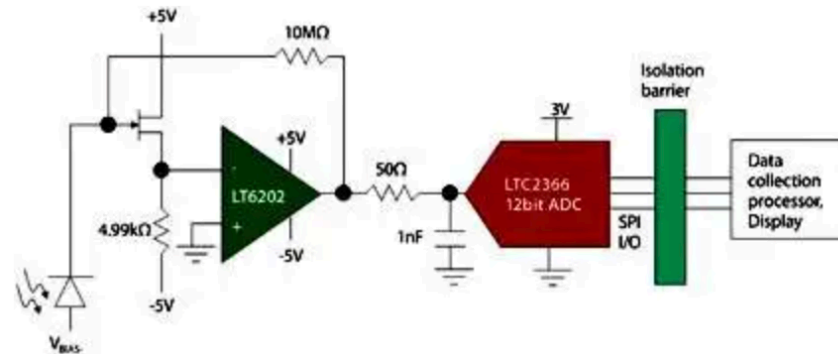
- Most ADC architectures (other than flash) are based on minimizing (reducing) the error between input and a D/A signal approximation
 - Pipeline uses distributed DAC
 - SAR ADC uses comparator to sense error
 - Sigma-delta ADC minimizes error via integration and feedback

SAR ADC



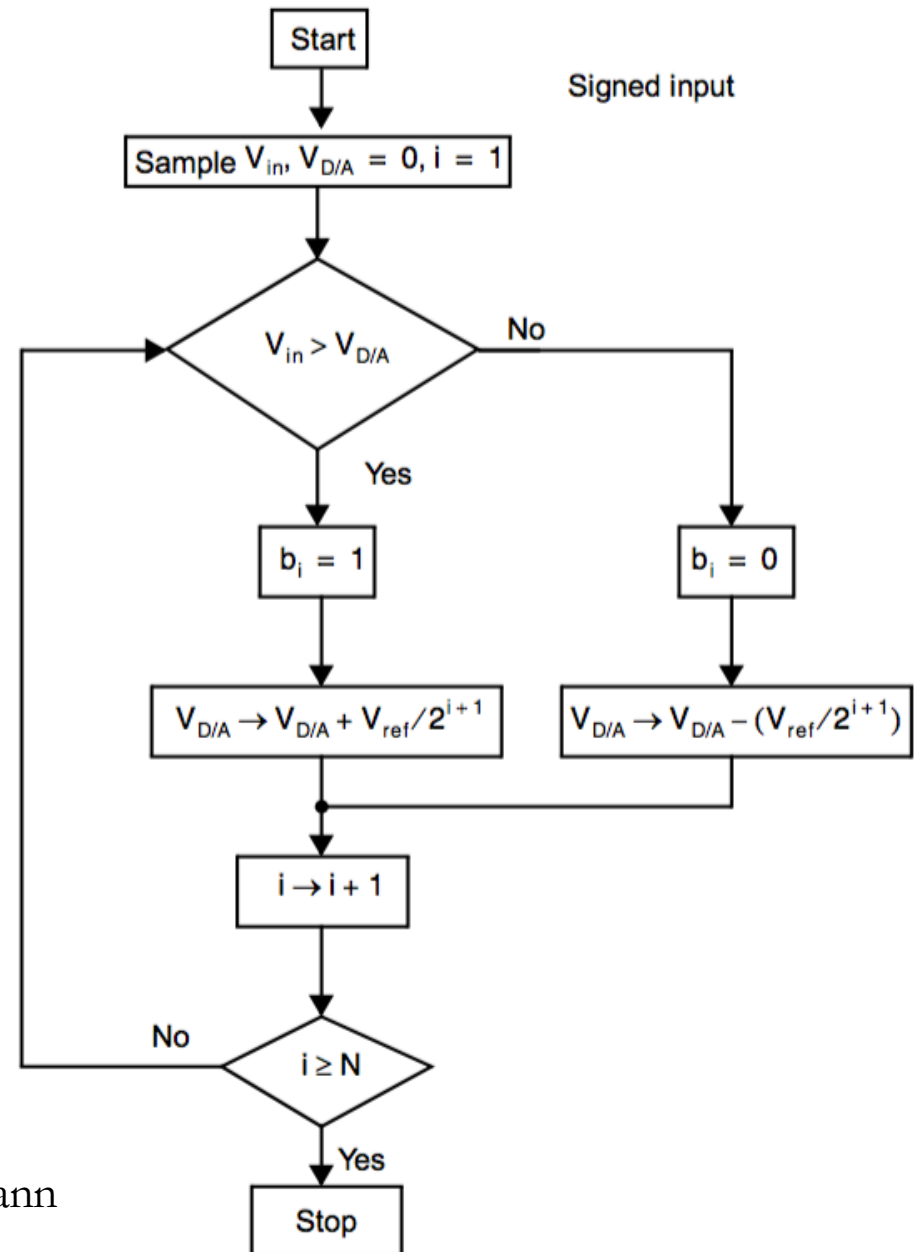
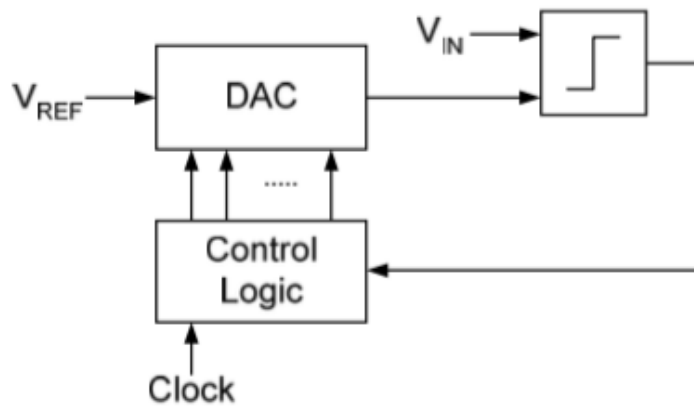
- ❑ Key features:
- ❑ High resolution
- ❑ Fast response and low latency
- ❑ Power varies with sample rate

Pulse Oximetry Example

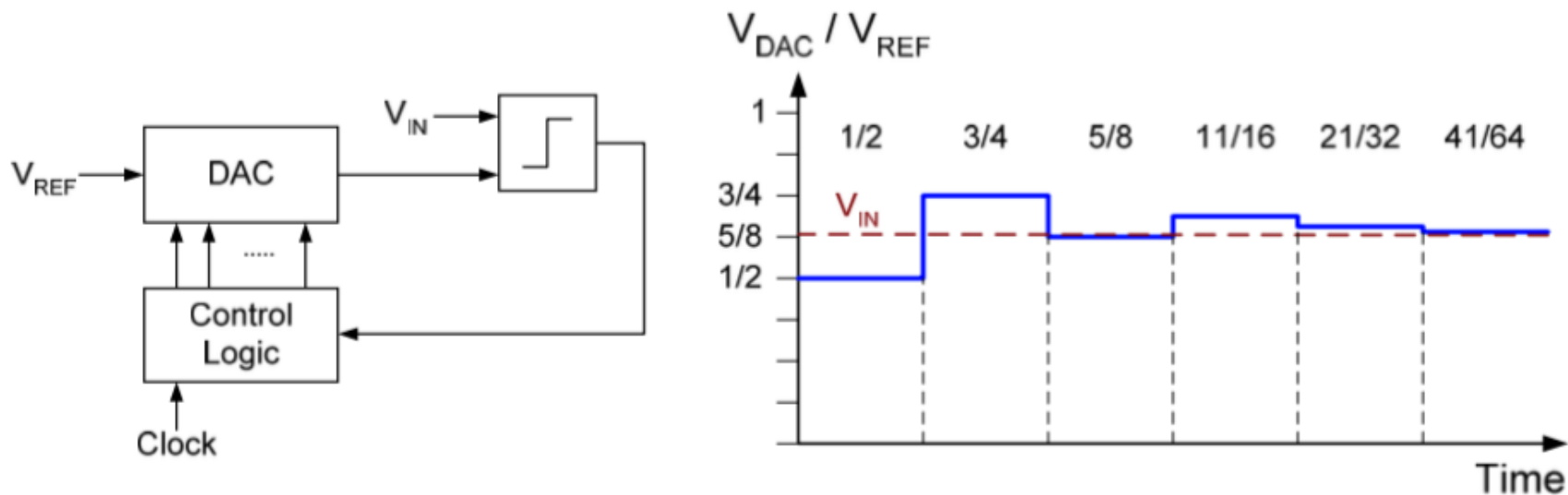


- ❑ LTC2366 is part of a family of tiny ADCs sampling from 100KSps to 3MSps
- ❑ ADCs dissipate only 7.8mW at 3MSps, 1.5mW at 100KSps and 0.3 microwatts in sleep mode
- ❑ LTC2366 features no data latency through the ADC

Successive Approximation Algorithm

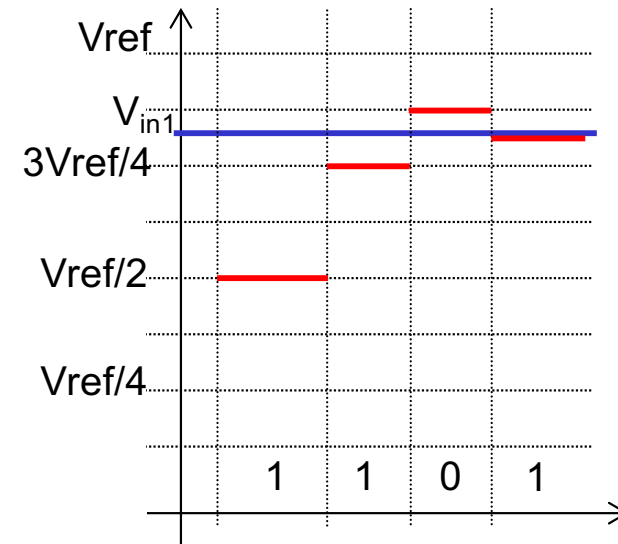
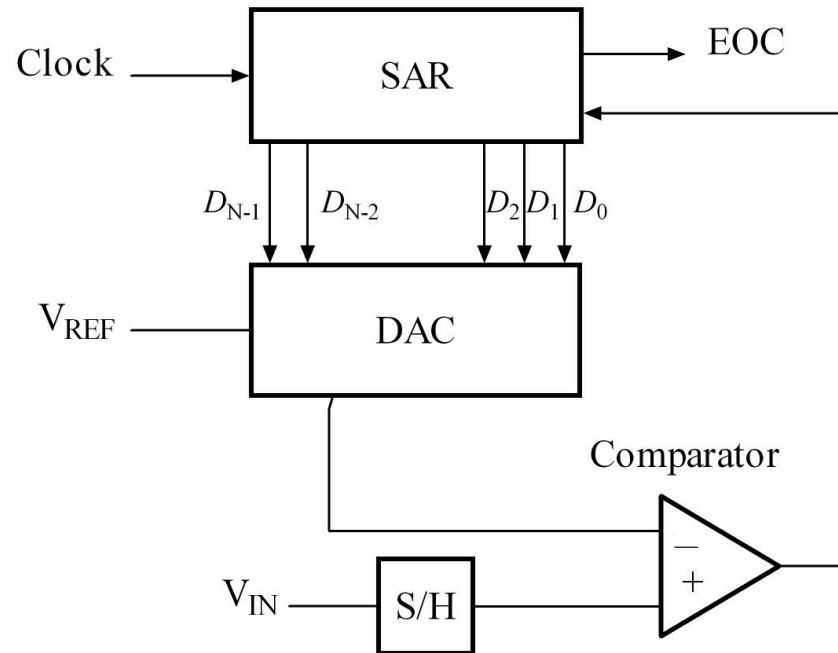


Successive Approximation Register ADC



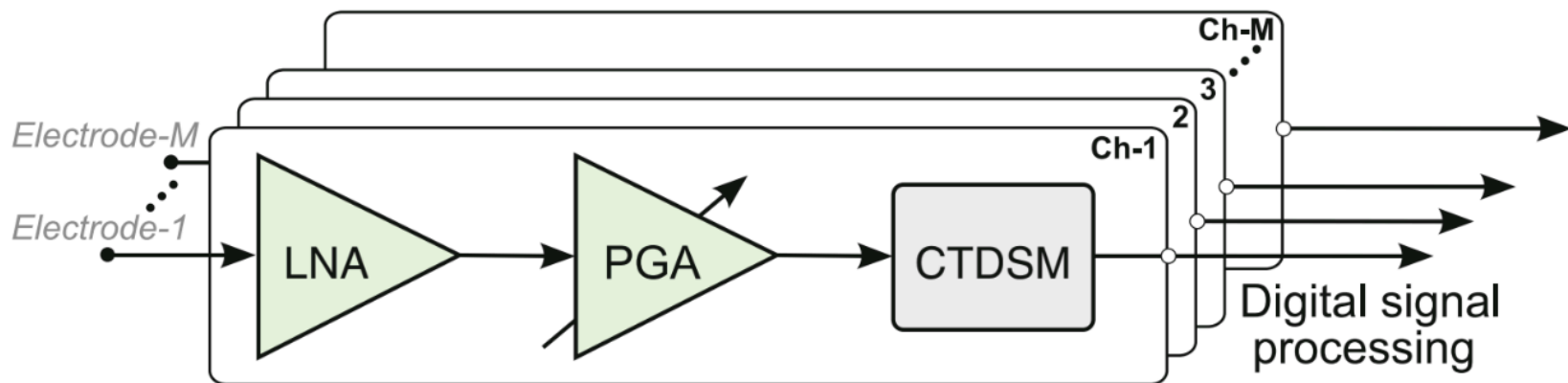
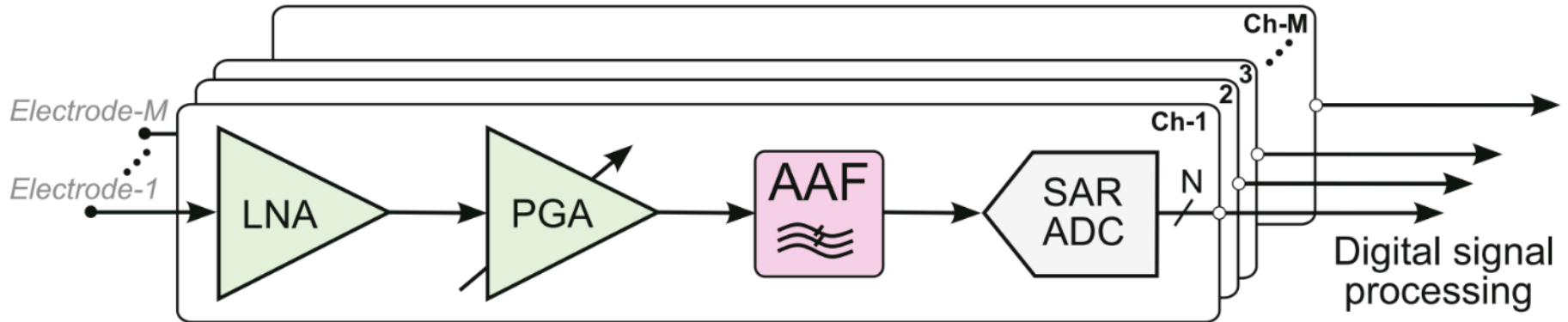
- ❑ Binary search over DAC output
- ❑ High accuracy achievable (16+ bits)
 - Relies on highly accurate comparator
- ❑ Moderate speed (1+ Mhz)

SAR ADC Block Diagram

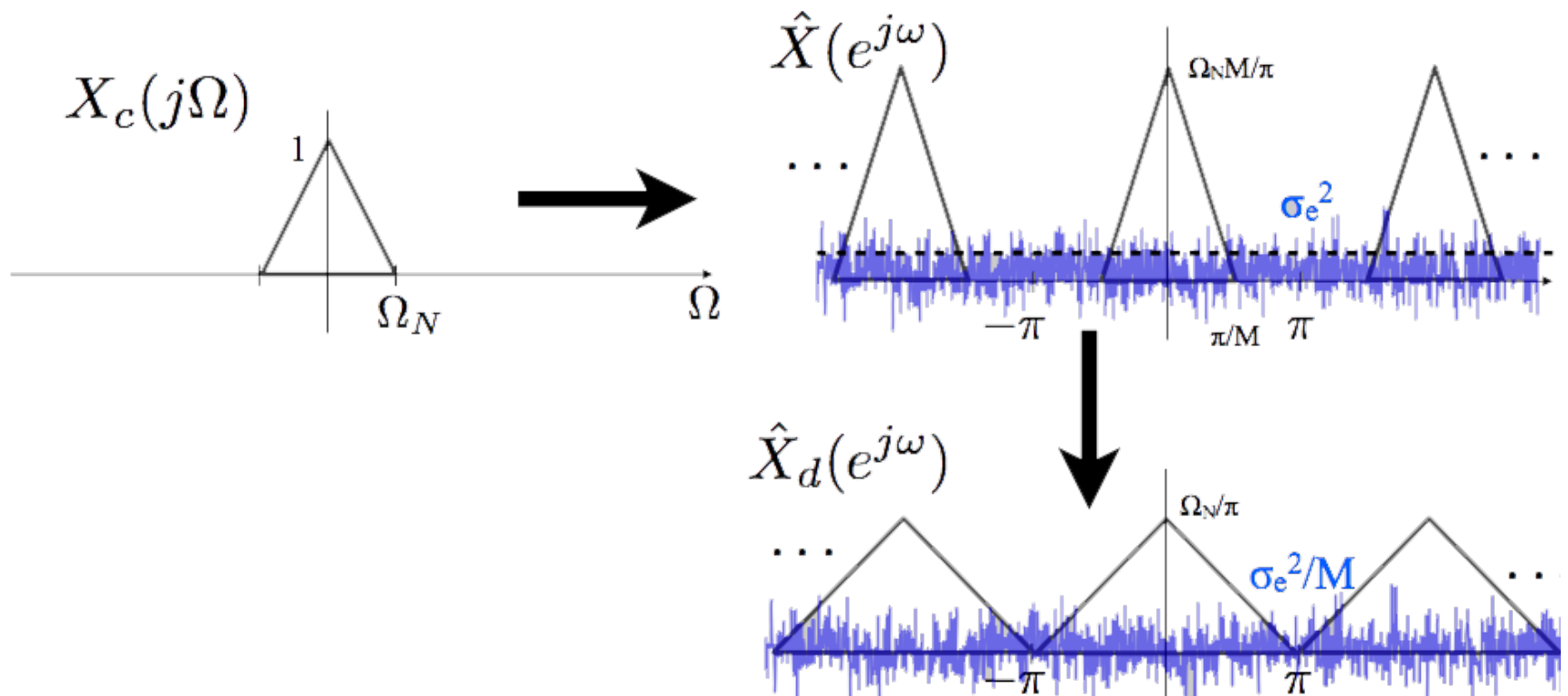
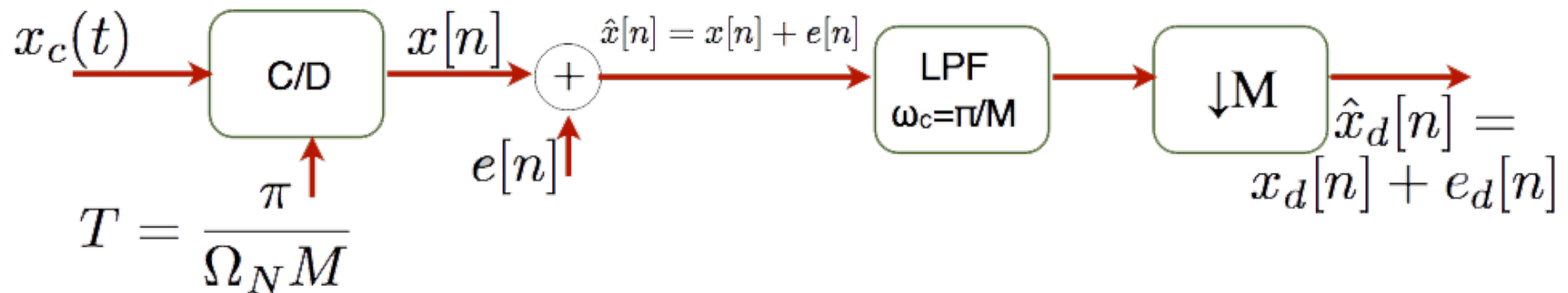


- ❑ Sampling phase: Sample input with Sample-and-Hold
- ❑ Bit-cycling: Compare with DAC output, adjusting the SAR with each clock cycle as bits are determined

Multi-channel Bio-potential Recording



Quantization Noise with Oversampling



Oversampled Converters Baseband Noise

$$S_B = S_{B0} \left(\frac{2f_B}{f_s} \right) = \frac{S_{B0}}{M}$$

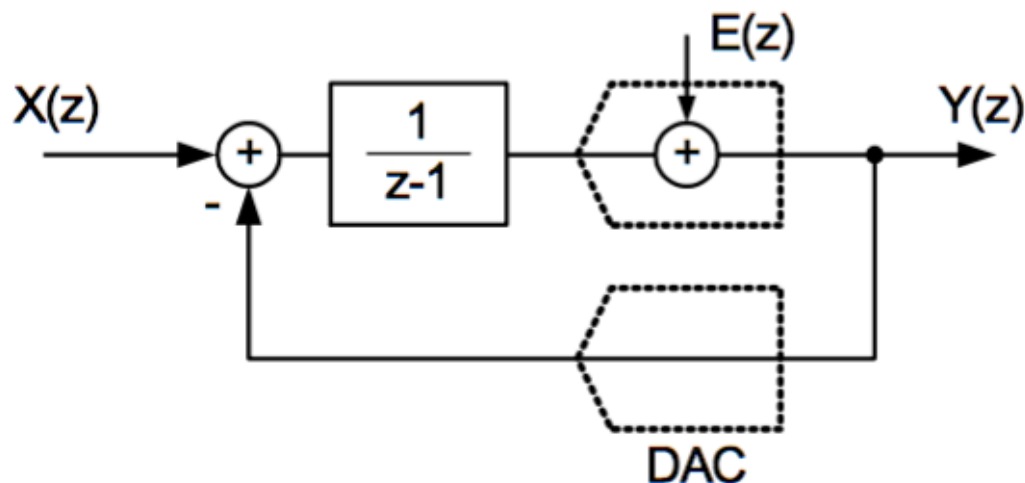
where $M = \frac{f_s}{2f_B} = \text{oversampling ratio}$

2X increase in M

→ 3dB reduction in S_B

→ 1/2 bit increase in resolution/octave oversampling

First Order Sigma-Delta Modulator



$$Y(z) = E(z) \frac{1}{1 + \frac{1}{z-1}} + X(z) \frac{\frac{1}{z-1}}{1 + \frac{1}{z-1}}$$
$$= E(z)(1 - z^{-1}) + X(z)z^{-1}$$

- Output is equal to delayed input plus filtered quantization noise

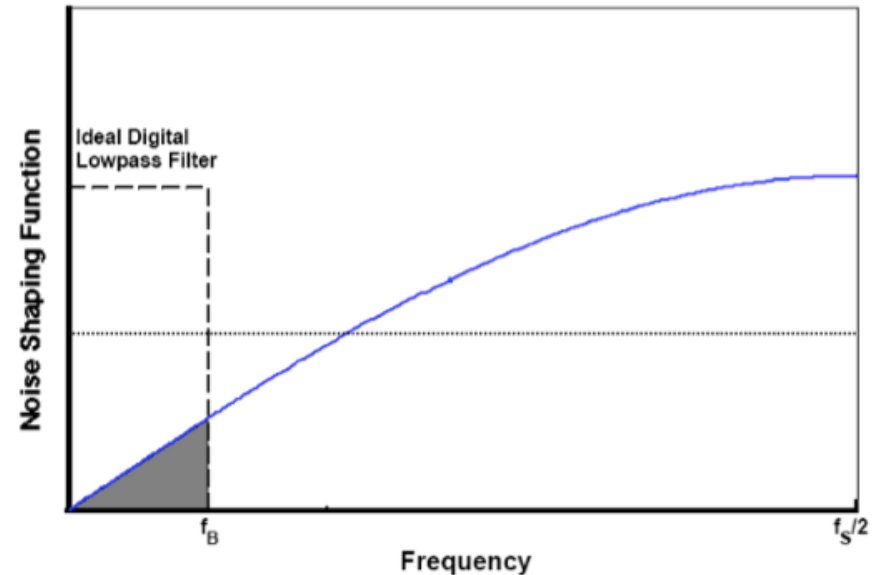
NTF Frequency Domain Analysis

$$H_e(z) = 1 - z^{-1}$$

$$H_e(j\omega) = (1 - e^{-j\omega T}) = 2e^{-j\omega T/2} \left(\frac{e^{j\omega T/2} - e^{-j\omega T/2}}{2} \right)$$

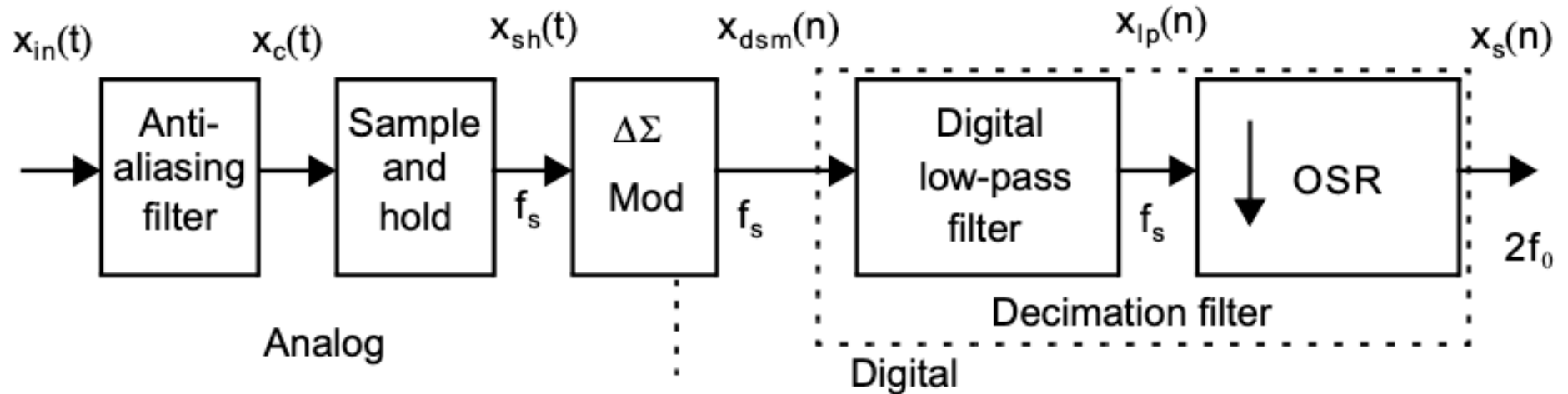
$$= 2e^{-j\frac{\omega T}{2}} \left(j \sin\left(\frac{\omega T}{2}\right) \right) = 2 \sin\left(\frac{\omega T}{2}\right) e^{-j\frac{\omega T - \pi}{2}}$$

$$|H_e(f)| = 2 \left| \sin(\pi f T) \right| = 2 \left| \sin\left(\pi \frac{f}{f_s}\right) \right|$$



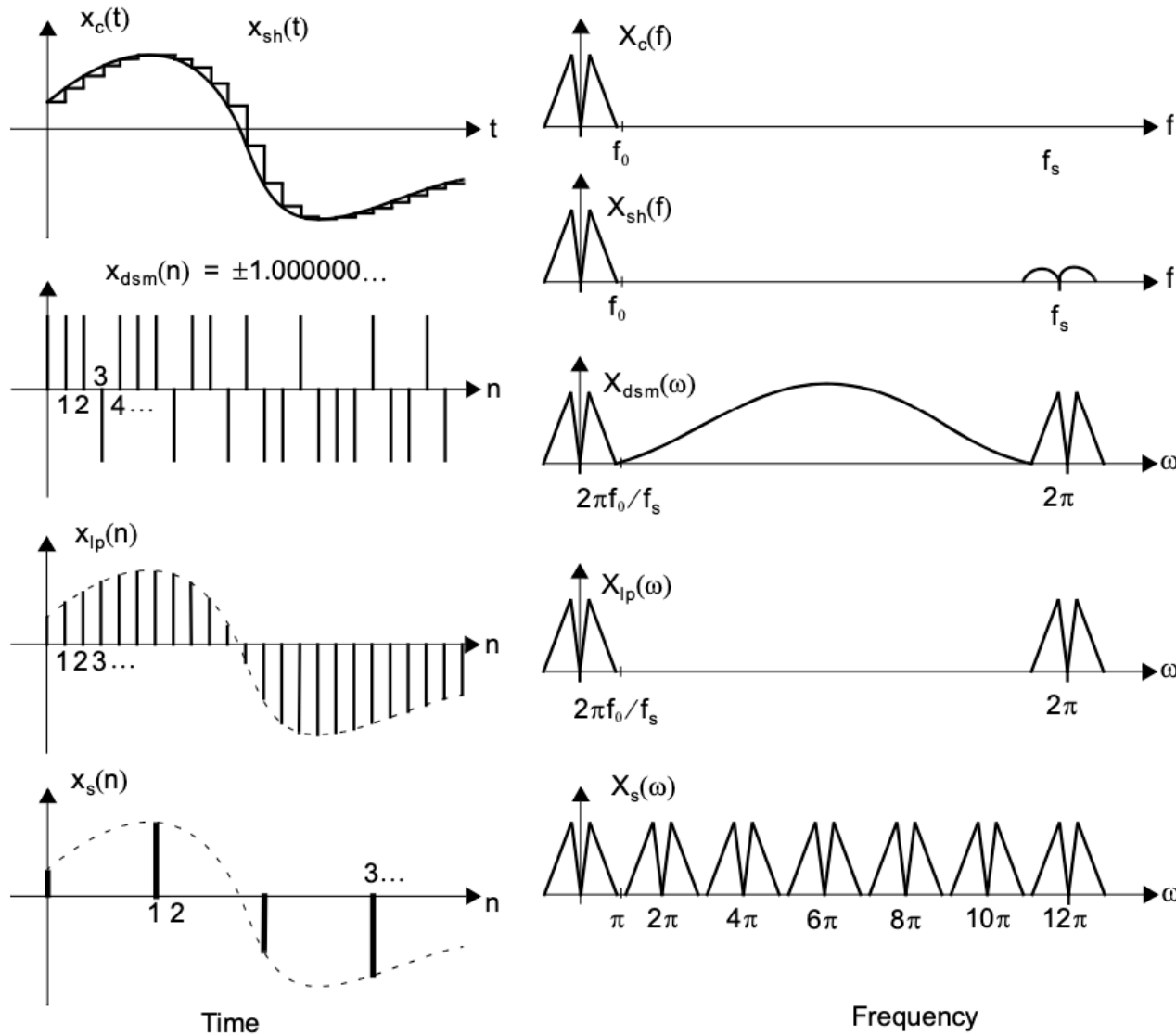
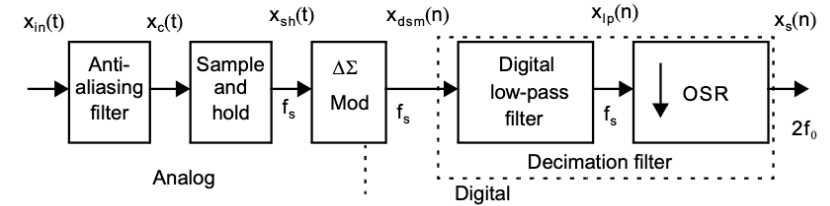
- "First order noise Shaping"
 - Quantization noise is attenuated at low frequencies, amplified at high frequencies

Decimation Filter

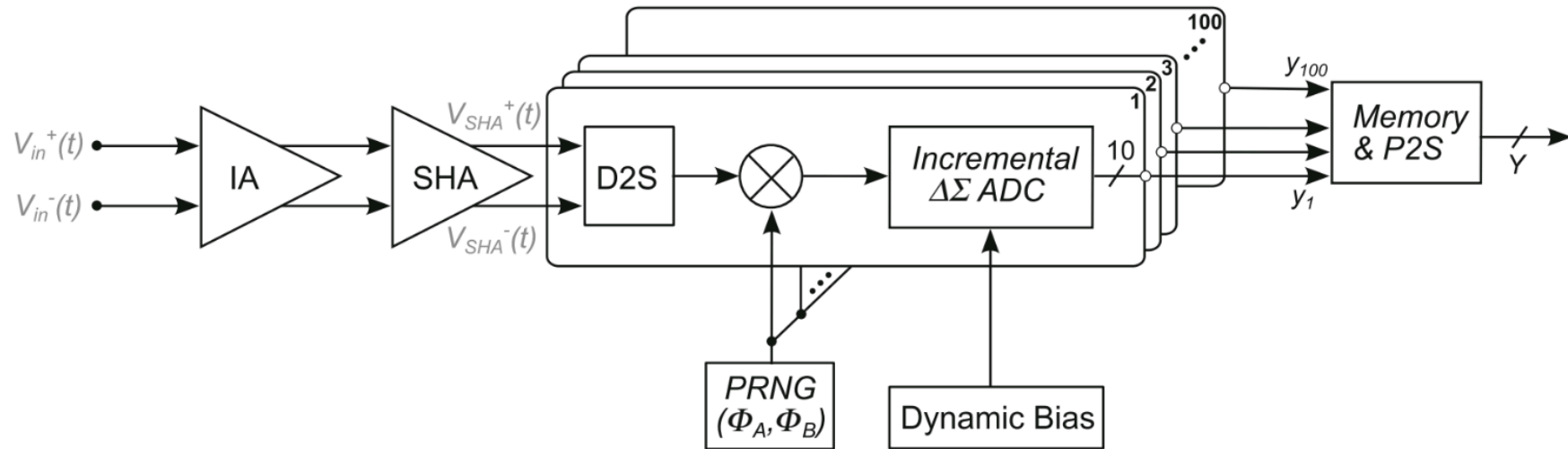




Decimation Filter



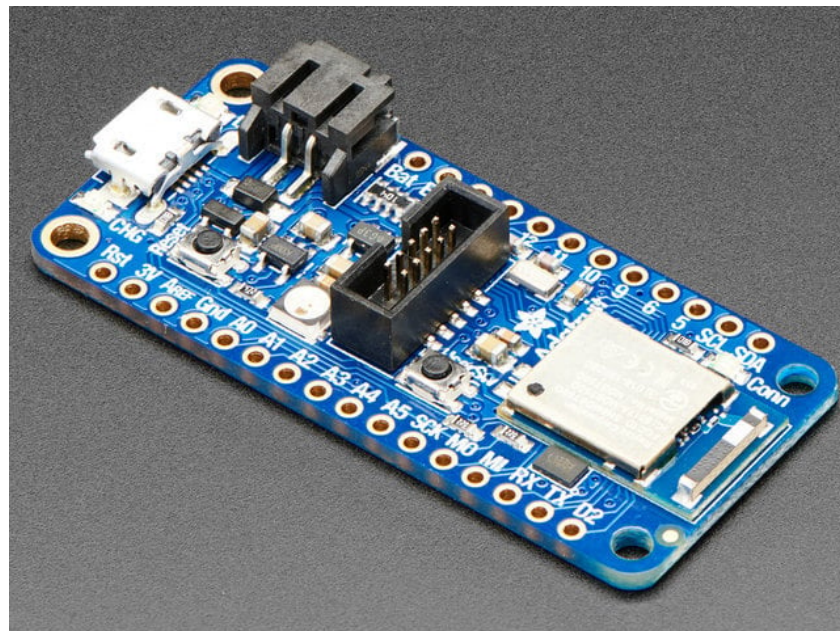
Compressed Sensing Front End for ECG Monitoring



- ❑ Compressive sensing allows fewer samples to recover signals exactly if signal is sparse.

Lab 6 – Data Converters

- ❑ The nRF52 family includes an adjustable 'successive-approximation ADC' which can be configured to convert data with up to 14-bit resolution (0..16383), and the reference voltage can be adjusted up to 3.6V internally.





Big Ideas

- ❑ DTFT vs DFT
 - The DFT characterizes the spectral content of the desired signals
- ❑ SQNR
 - SQNR determined by bit resolution, B
 - ENOB determined by SNR
- ❑ Oversampling
 - Enables reduction in quantization noise and reduces stress on AAF.
More next lecture...
- ❑ ADC Architectures
 - Flash ADCs - Word-at-a-time for high speed, low resolution applications
 - SAR ADC - Bit-at-a-time for low speed, low power applications
 - Sigma-Delta ADCs - Usually for low speed, low power applications



Admin

- ❑ Monday: Data Converter Lab
- ❑ Wednesday: Quiz 1
 - Designed for an hour, but you have the full 1.5 hour
 - Covers Lec 1-5 and Labs 1-5