

Balance recovery in the double support phase during perturbed walking

M. van Mierlo, M. Vlutters, H. van der Kooij & E. H. F. Asseldonk

Background & Aim

- Exoskeletons have a very slow walking speed.
- Slow walking increases duration of the double support phase (DSP).
- Crucial to control balance when both feet are on the ground.
- The centre of pressure (CoP) describes the control of the centre of mass (CoM) movement [1].

How do modulations of the CoP trajectory contribute to the control of the CoM during the double support phase?

Experimental data

- 10 subjects walking at 1.25 ms^{-1} [2]
- Pelvis perturbations at toe-off right
- Magnitude 4, 8, 12, 16 % of body weight

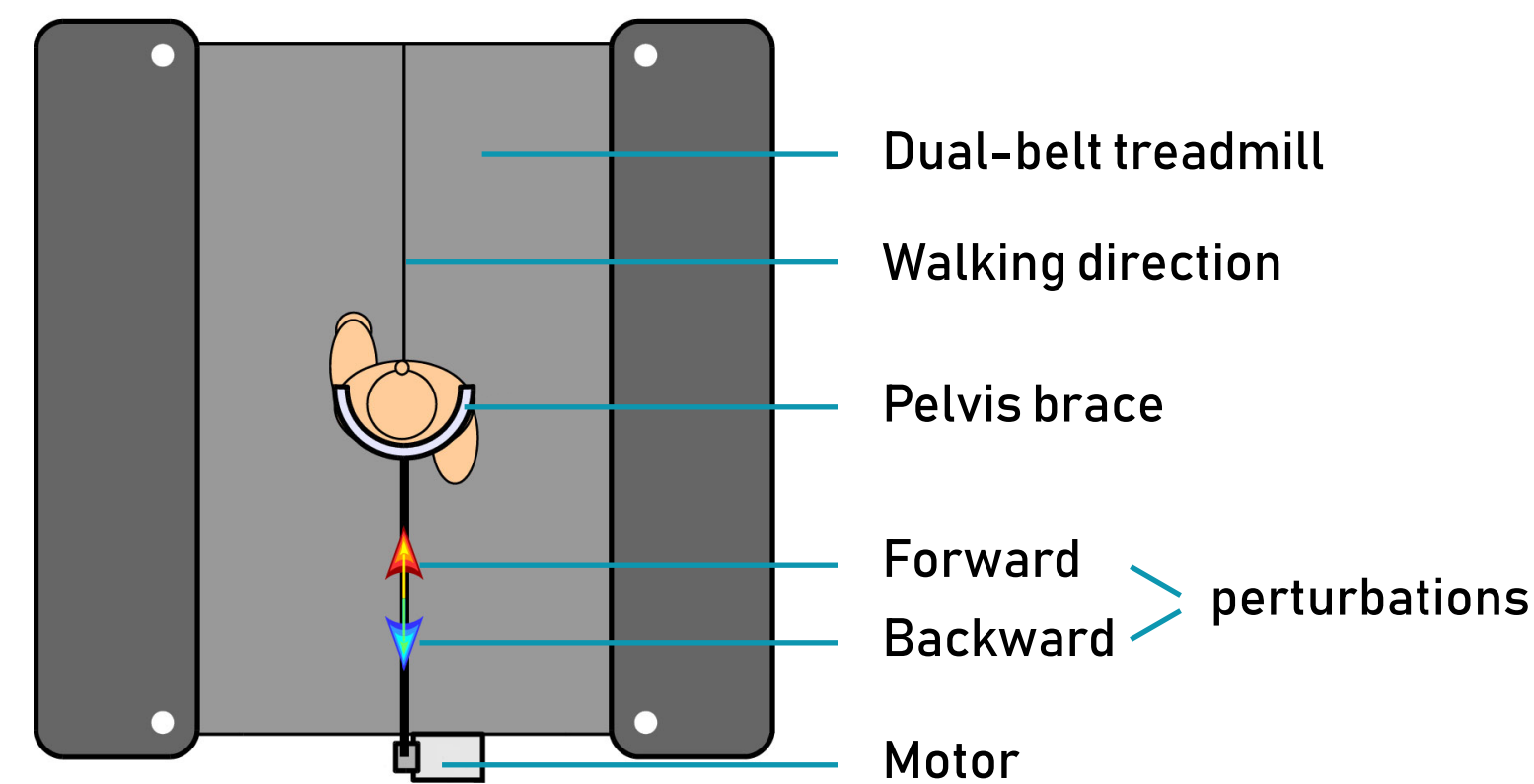


Figure 1: Experimental setup. [2]

Methods

Modelled data

Simple inverted pendulum model [3]:

- Input: Generated CoP trajectories
- Output: CoM position and velocity

$\Delta \text{CoM velocity} = \text{end} - \text{begin velocity of the DSP}$

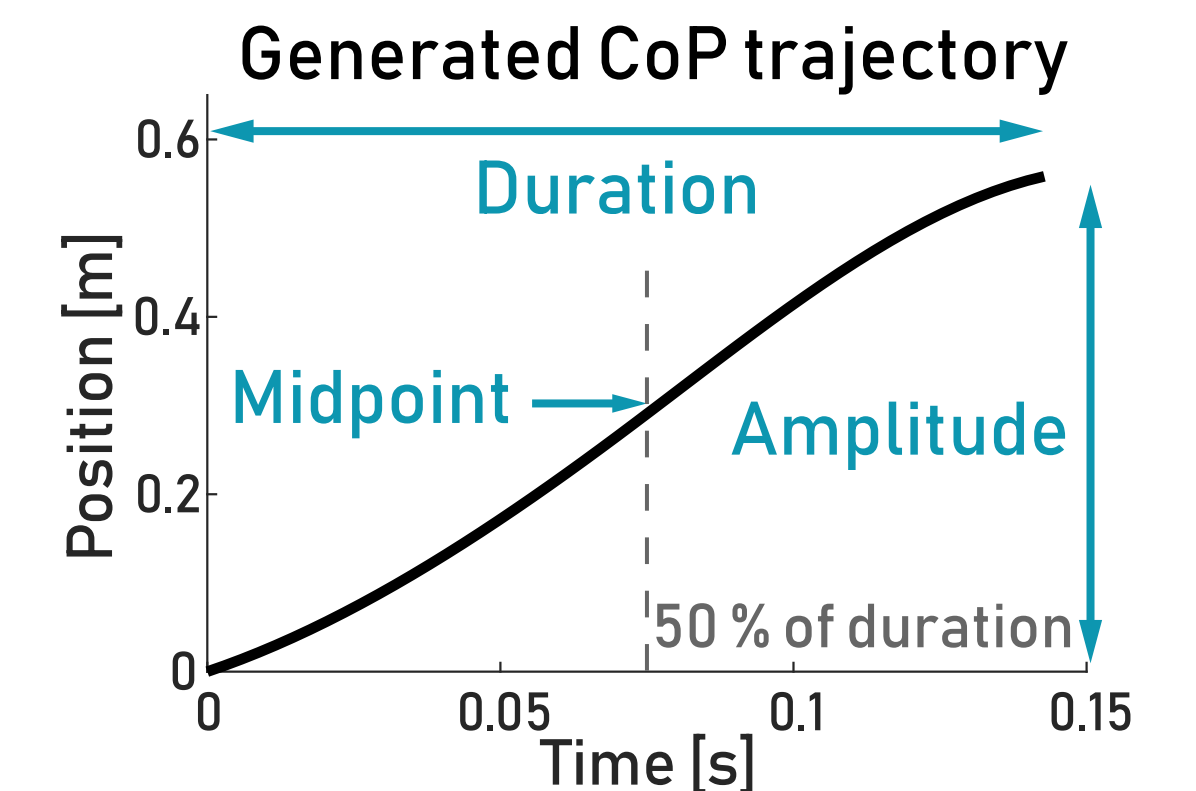


Figure 2: Parameterised CoP trajectories, based on spline.

Results

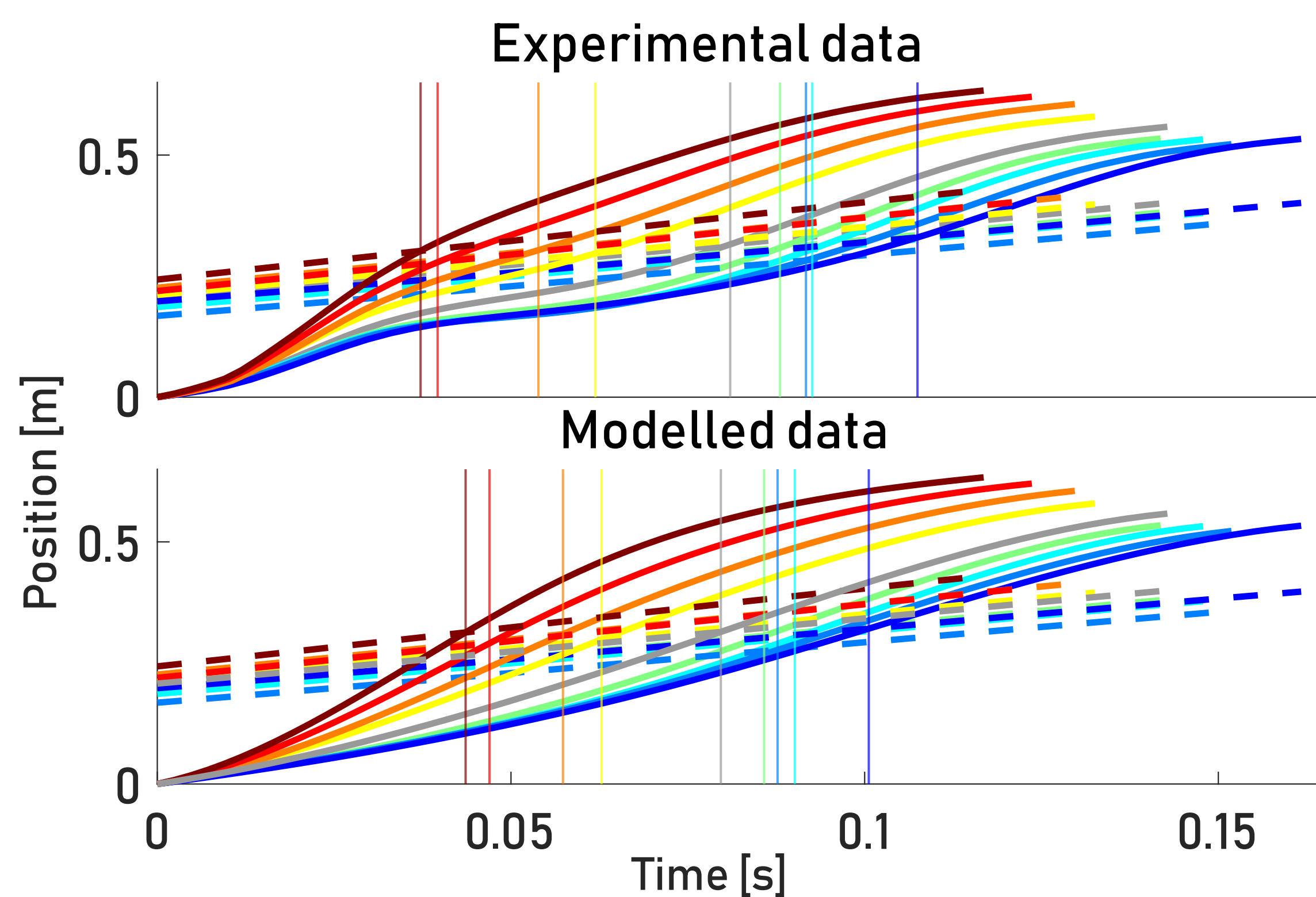


Figure 3: Top) Experimental CoP and CoM trajectories for different perturbation magnitudes. Bottom) Generated CoP trajectories based on values from experimental data and modelled CoM trajectories.

- Minimal difference between the end CoM position of the experimental and modelled data: 0.1 – 0.4 mm
- Systematically lower ΔCoM velocities for modelled data: 0.1 – 95 mm/s

Experimental data

Perturbation magnitudes:

- Baseline
- Forward 16%
- Forward 12%
- Forward 8%
- Forward 4%
- Backward 4%
- Backward 8%
- Backward 12%
- Backward 16%
- CoP
- CoM
- | Cross CoM CoP

All data is presented in the sagittal plane.

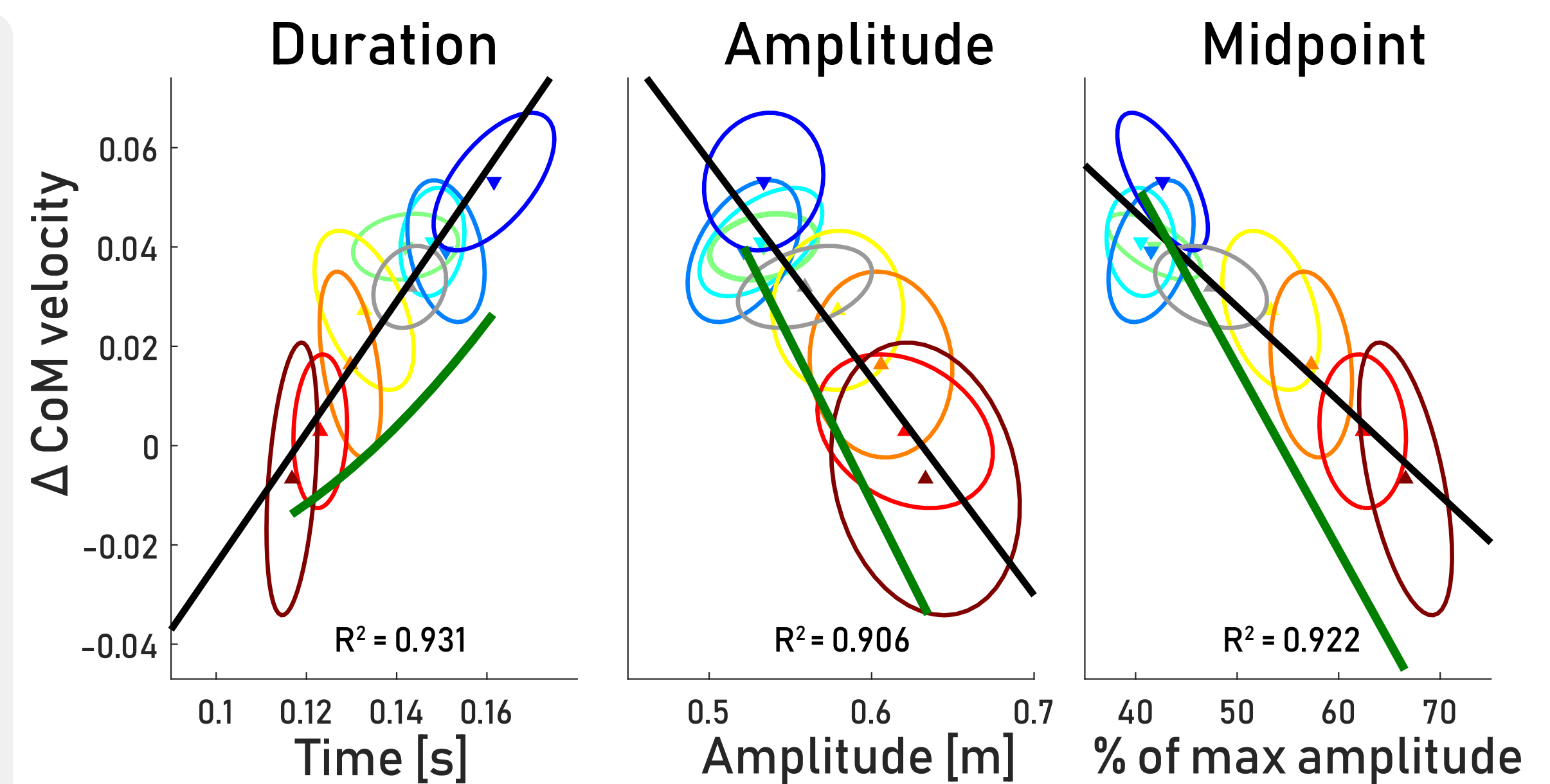


Figure 4: Relationships between CoP parameters and ΔCoM velocity for experimental (triangles with ellipses [mean \pm std] and LLSQ fit [black line and R^2 value]) and modelled data (green line).

Experimental data

- Linear relationships between the ΔCoM velocity and all CoP parameters.

Modelled data

- Directions of relationships correspond with experimental data.
- Systematically lower ΔCoM velocity compared to experimental data.

Conclusion

- A simple inverted pendulum model is able to model representative CoM trajectories during the DSP, from a generated input CoP trajectory using only three CoP parameters.
- Subjects used all the CoP parameters, the duration, amplitude and midpoint, to control the CoM velocity after a perturbation.
- Earlier or later loading the leading leg helped in controlling the CoM velocity, and was even more effective than changing the duration or amplitude.

References

- [1] H. Reimann, T. D. Fettrow, E. D. Thompson, P. Agada, B. J. McFadyen, and J. J. Jeka, "Complementary mechanisms for upright balance during walking," *PLoS One*, vol. 12, no. 2, pp. 1–16, 2017.
- [2] M. Vlutters, E. H. F. van Asseldonk, and H. van der Kooij, "Center of mass velocity-based predictions in balance recovery following pelvis perturbations during human walking," *J. Exp. Biol.*, vol. 219, no. 10, pp. 1514–1523, 2016.
- [3] Y. Jian, D. Winter, M. Ishac, and L. Gilchrist, "Trajectory of the body COG and COP during initiation and termination of gait," *Gait Posture*, vol. 1, no. 1, pp. 9–22, 1993.



This work is part of the research program Wearable Robotics with project number P16-05, which is (partly) funded by the Dutch Research Council (NWO)

UNIVERSITY OF TWENTE | TECHMED CENTRE